

# Fields of Dreams: Modeling and Analysis of Large Scale Activity in the Brain

Bard Ermentrout

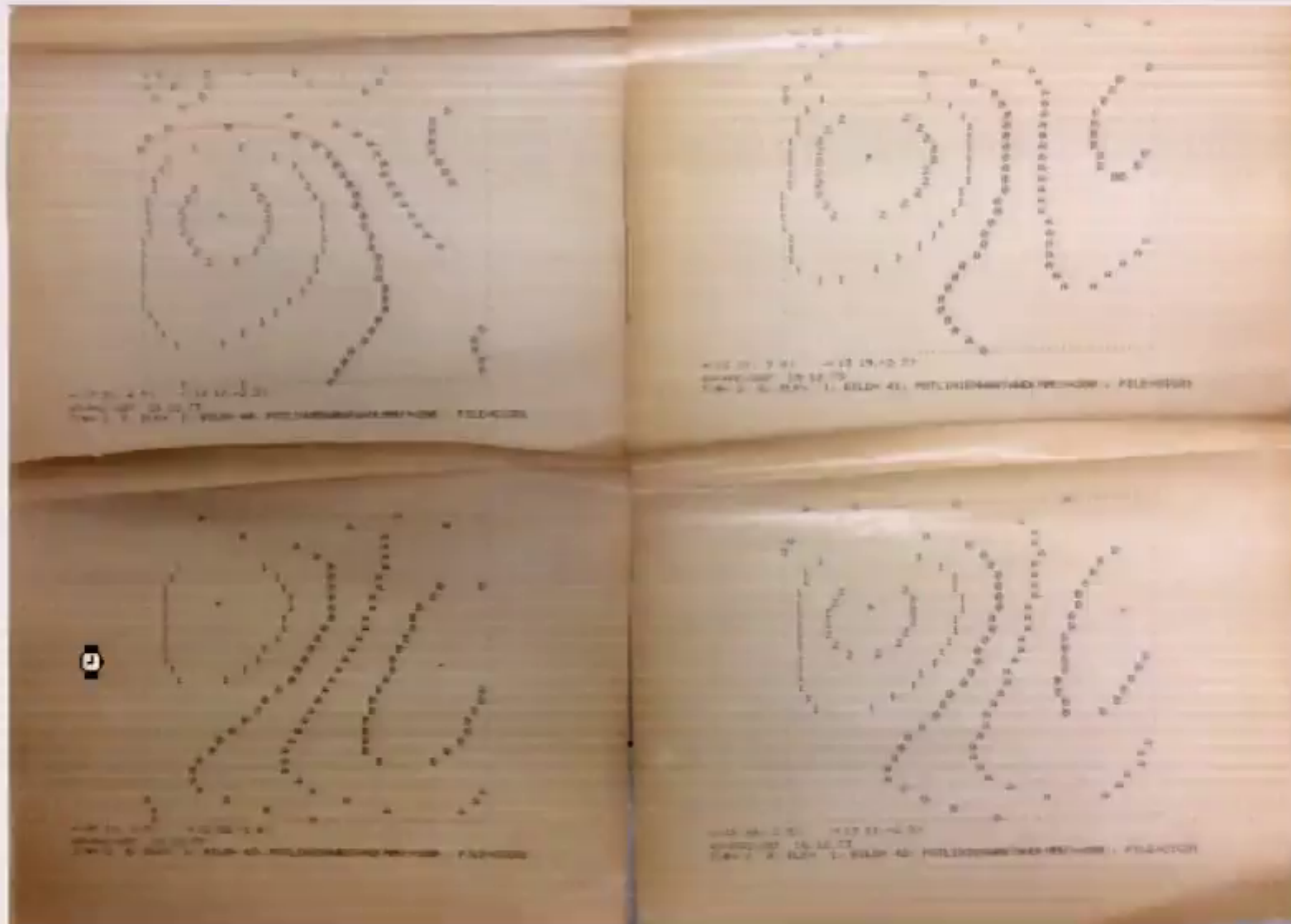
University of Pittsburgh

May 18, 2015

# OUTLINE

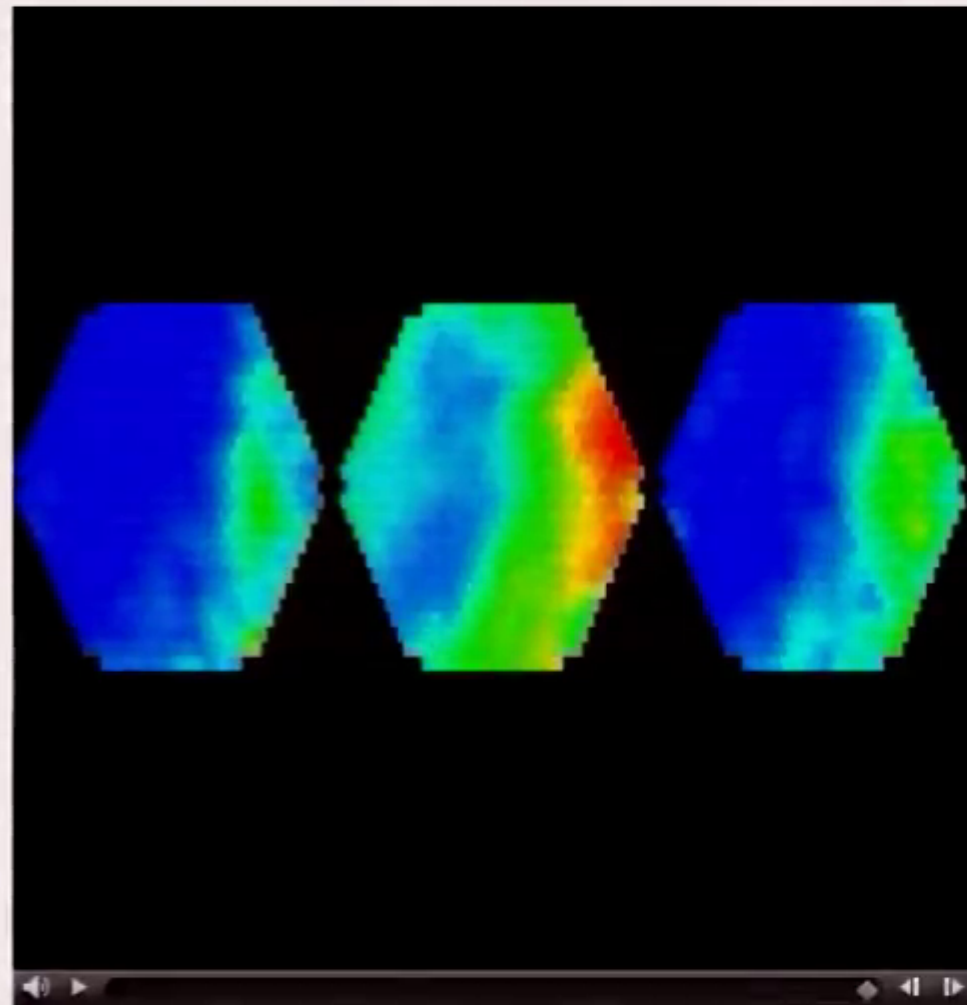
- Examples and methods of recording spatio-temporal activity
- Data analysis and challenges
- Meaning of the activity
- Approaches to modeling
- Mathematical challenges

# PETSCHKE & RAPPELSBERGER, 1973



# SPATIO-TEMPORAL NEURAL PATTERNS

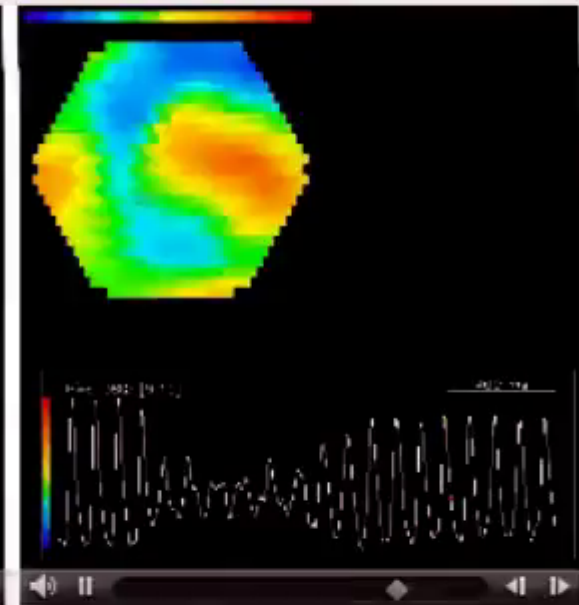
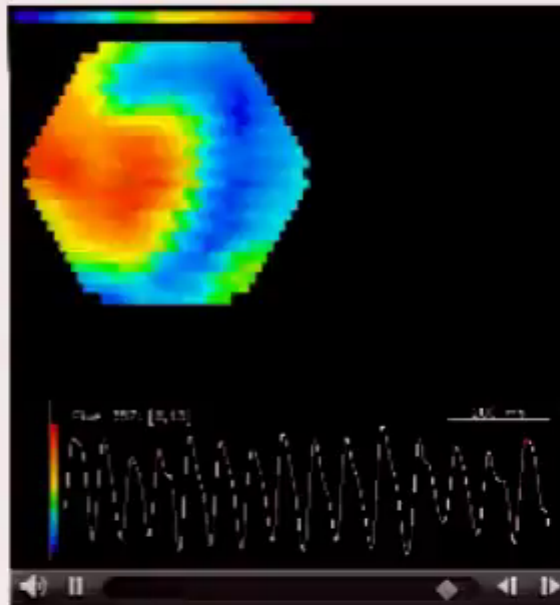
- Reflected waves  
(Wu lab)





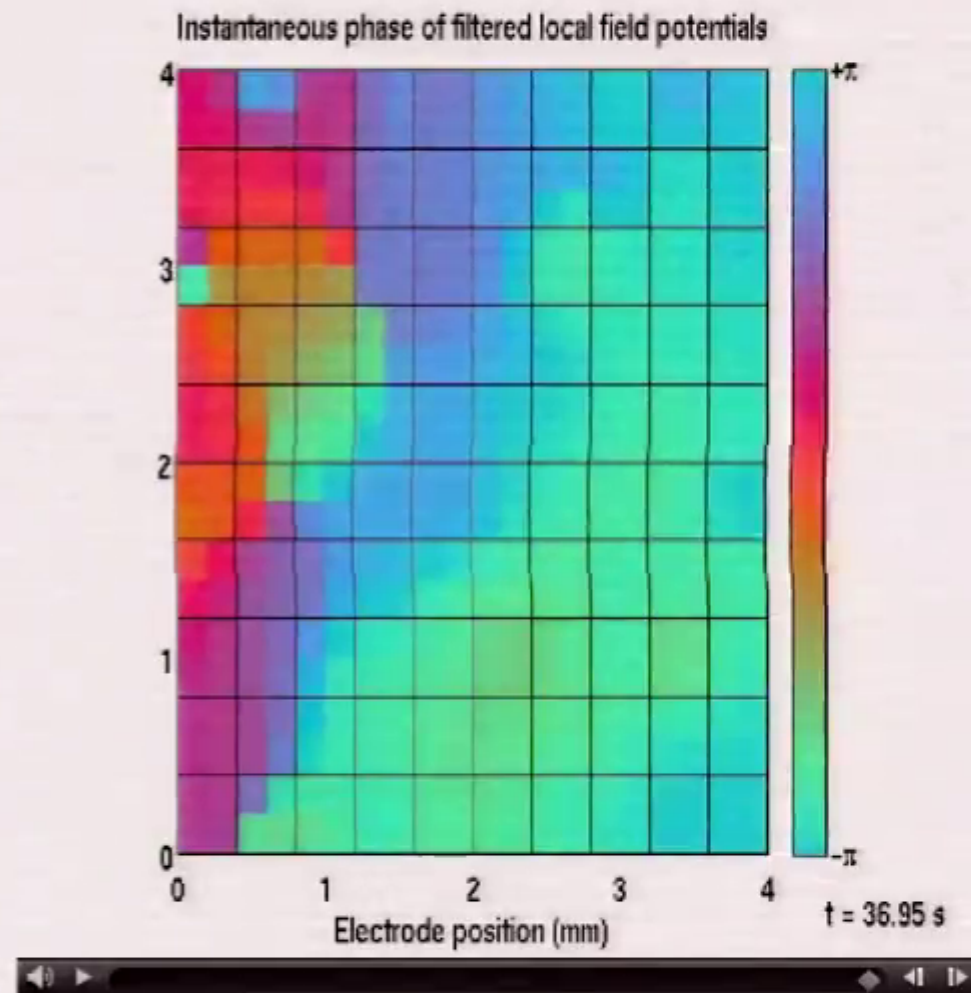
# SPATIO-TEMPORAL NEURAL PATTERNS

- Reflected waves
- Rotating waves (Wu lab)



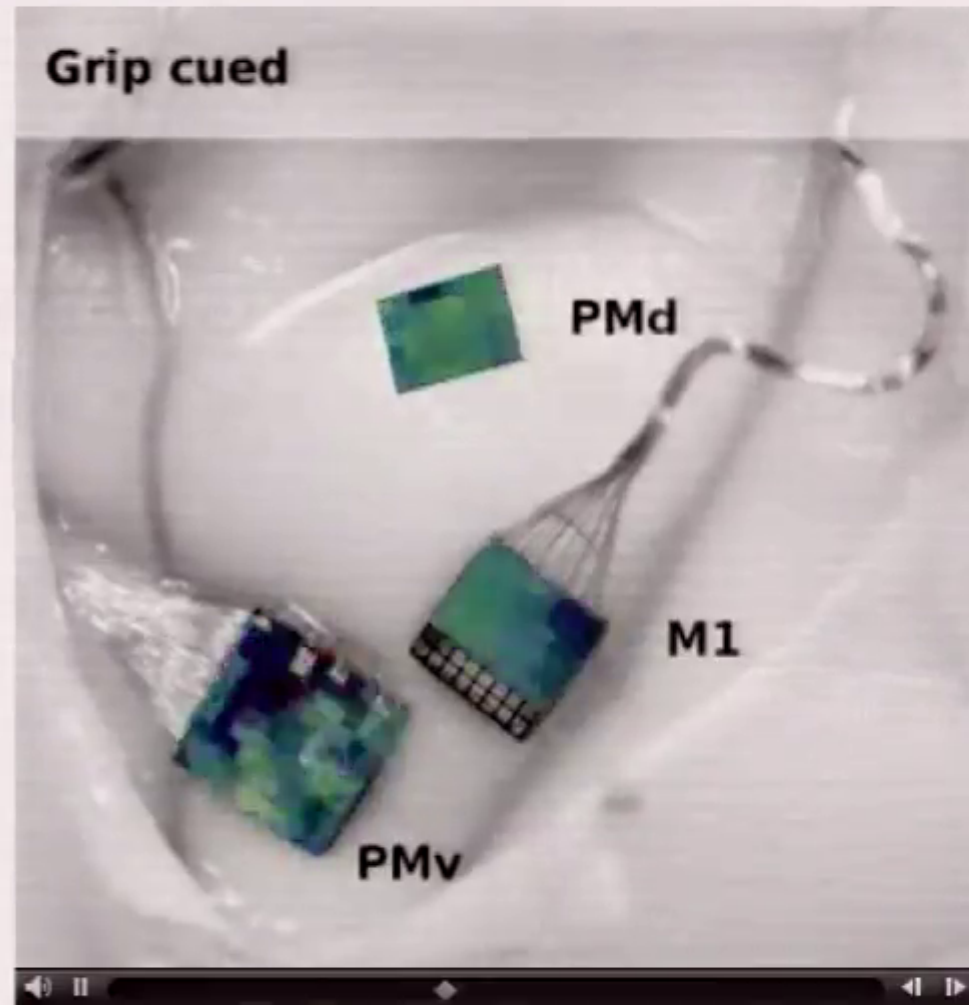
## SPATIO-TEMPORAL NEURAL PATTERNS

- Reflected waves
- Rotating waves
- Complex patterns in V1 (PG)



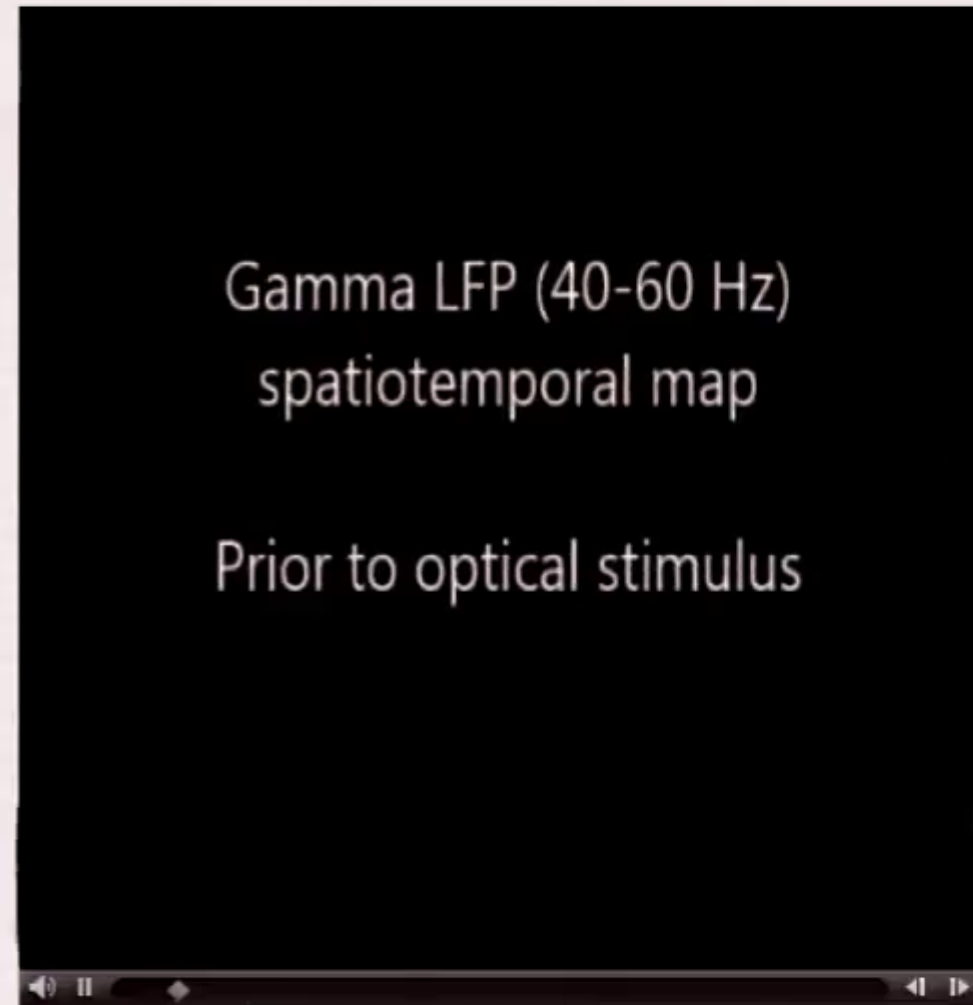
# SPATIO-TEMPORAL NEURAL PATTERNS

- Reflected waves
- Rotating waves
- Complex patterns in V1
- Complex Motor ctx patterns (WT)



# SPATIO-TEMPORAL NEURAL PATTERNS

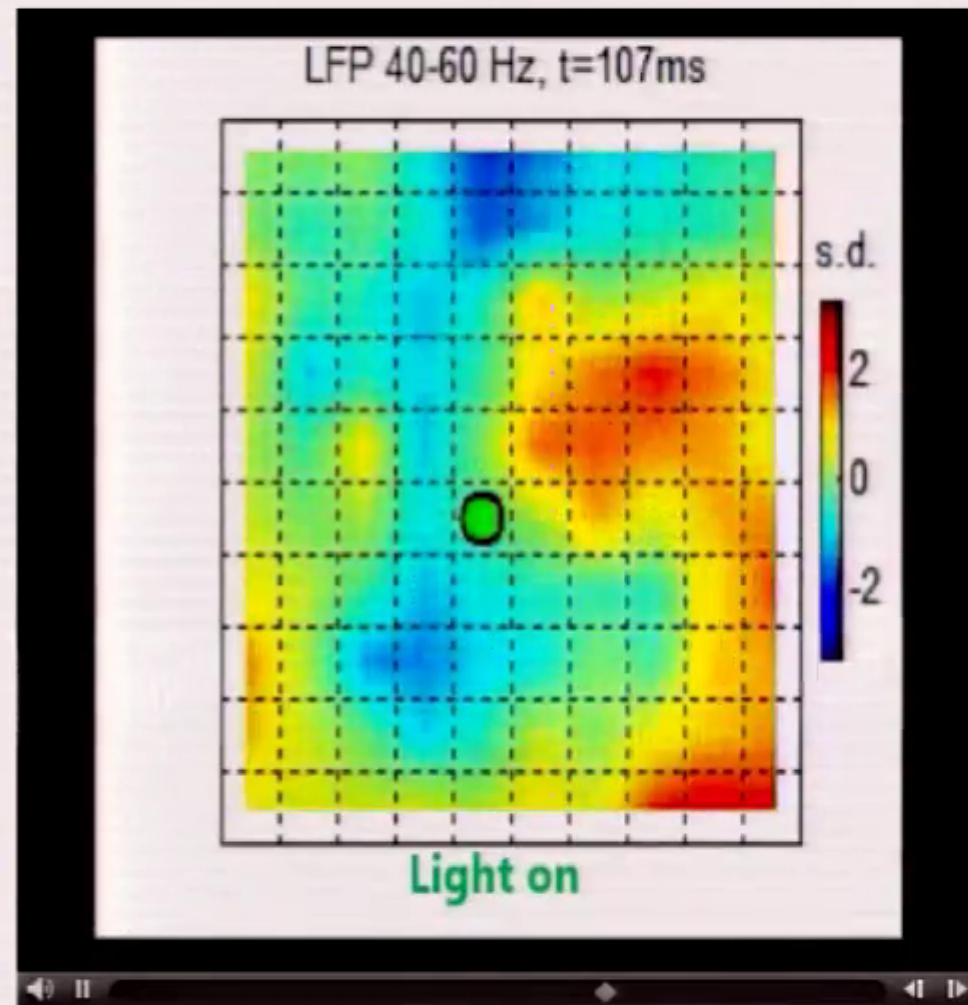
- Reflected waves
- Rotating waves
- Complex patterns in V1
- Complex Motor ctx patterns
- Stimulus induced patterns (WT)





## SPATIO-TEMPORAL NEURAL PATTERNS

- Reflected waves
- Rotating waves
- Complex patterns in V1
- Complex Motor ctx patterns
- Stimulus induced patterns (WT)





# ANALYSIS/VISUALIZATION OF SPATIO-TEMPORAL DATA

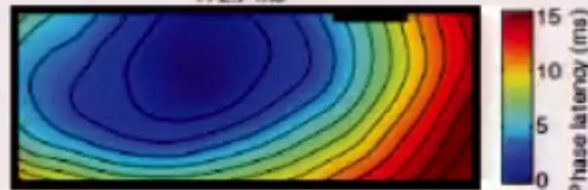
- Filter at different frequency bands
- Conversion to phase using Hilbert transform
- Extract something from this (?)
  - Fit to plane-waves or rotating waves
  - Phase latency extraction (Muller et al, 2014)
  - Gong et al use methods from fluid dynamics

# PHASE-LATENCY

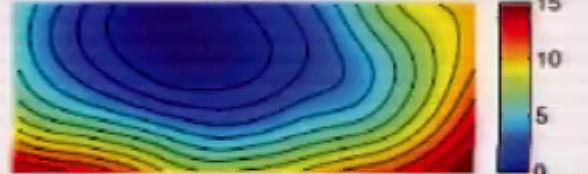
+155 ms



**a** Stimulus evoked  
+72.7 ms



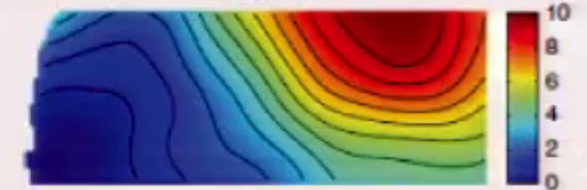
+72.7 ms



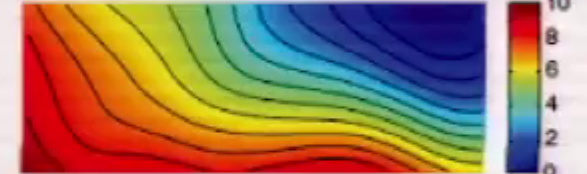
+72.7 ms



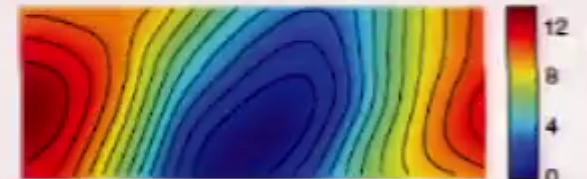
**b** Spontaneous  
+54.5 ms



+145.4 ms



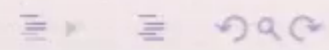
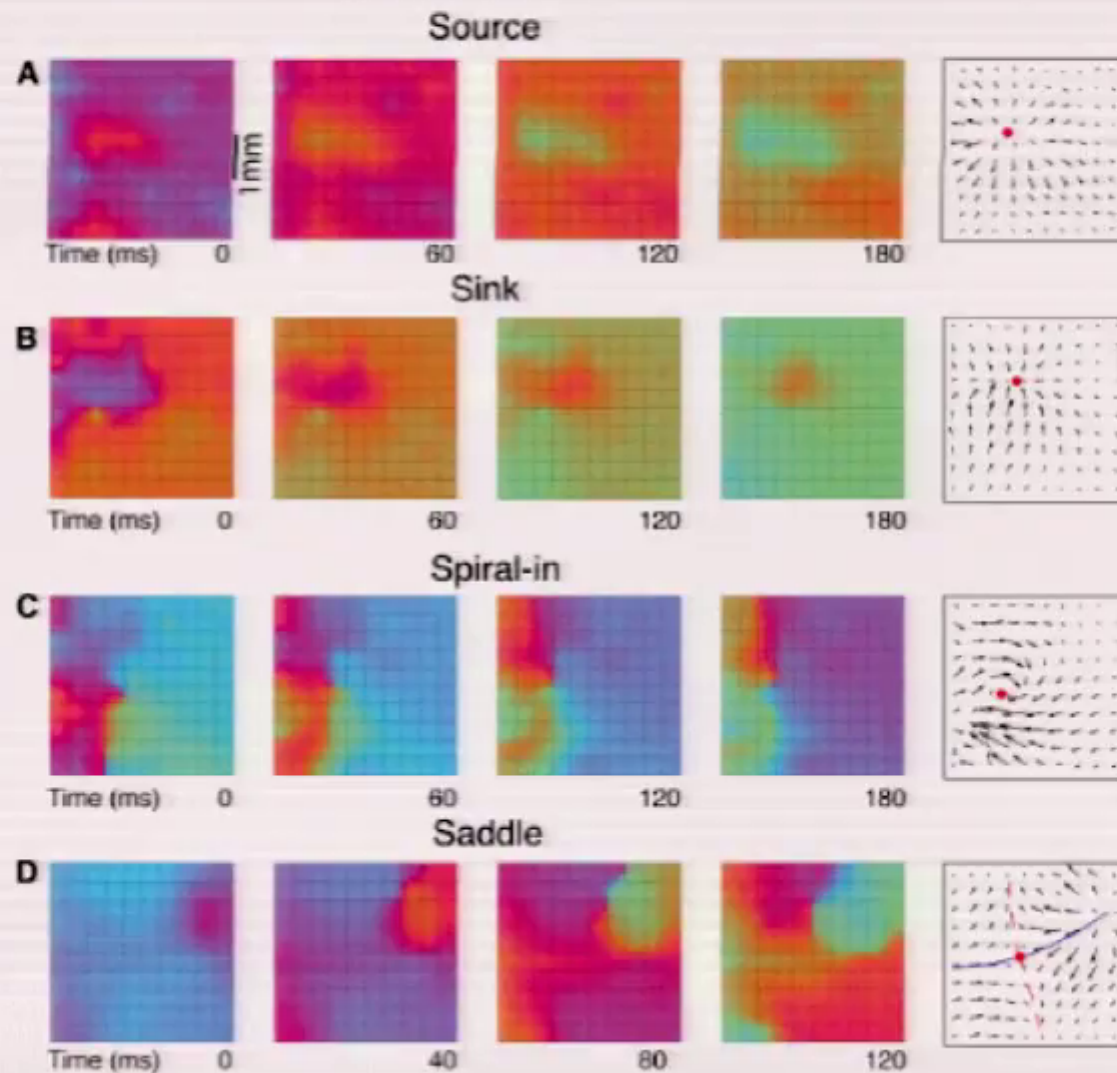
+36.4 ms



# COMPLEX WAVES IN MT OF MARMOSET

Townsend et al. • Complex Cortical Waves

J. Neurosci., March 18, 2015 • 35(11):4657–4662 • 4659



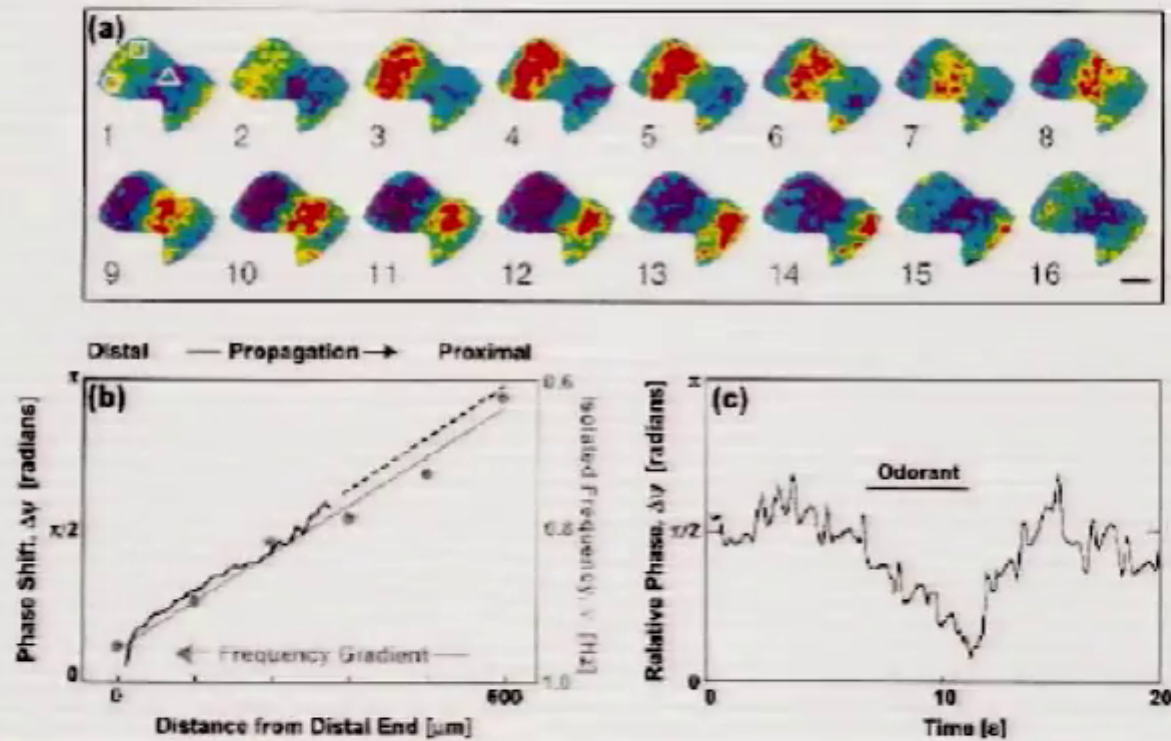
## COMPUTATIONAL ROLE

- Do these patterns have a computational role or are they “the exhaust fumes of computation?”
- Several theories of the “meaning” of waves
- Can reflect evoked activity
- May set biases – providing a mechanistic view of Bayesian computations
- Could also be the basis for the actual computation (as in WM)



# WAVES & MEMORY

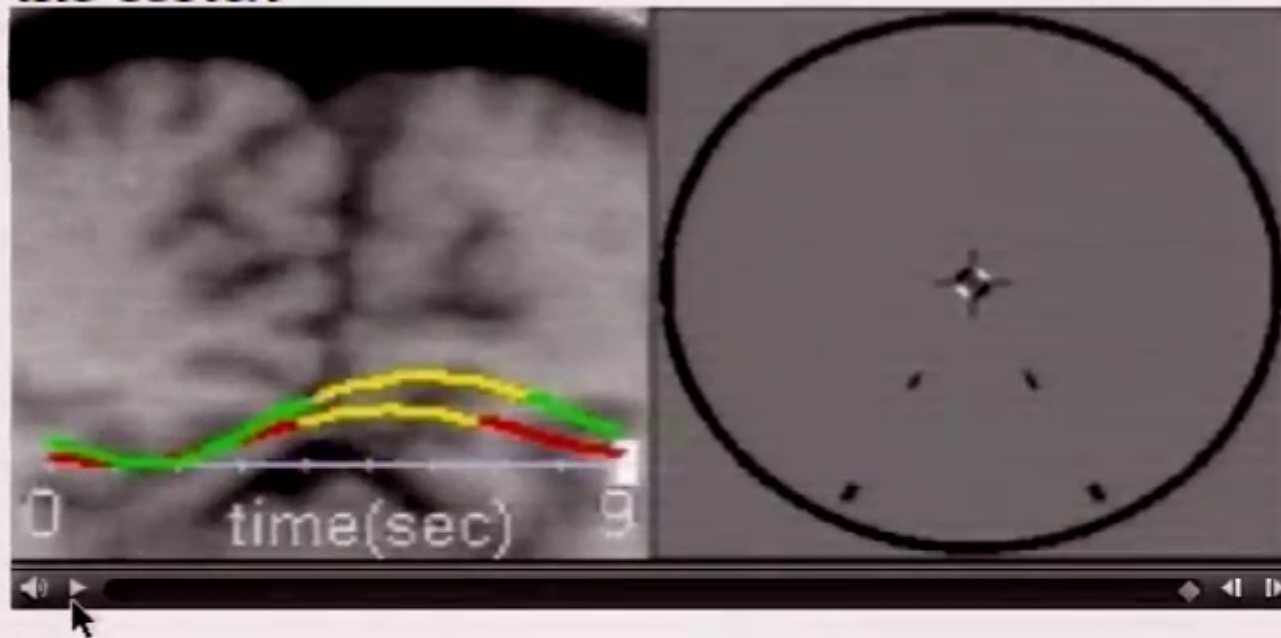
David Kleinfeld & I suggested that they could set up a position code in the *Limax* olfactory lobe





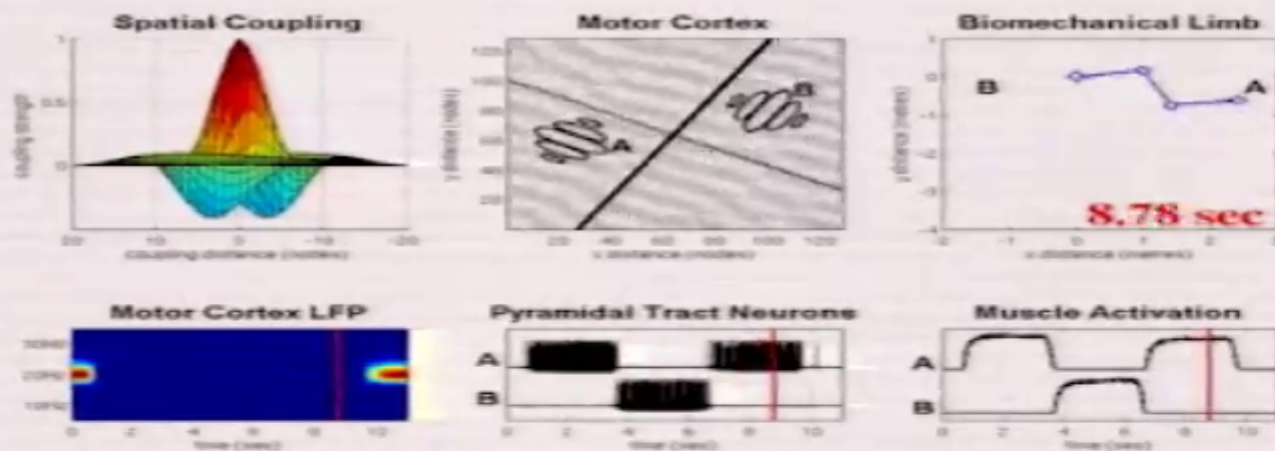
# WAVES & RIVALRY

When the visual system receives two conflicting images, it picks a winner, but switches back and forth between the two (*Binocular rivalry*). In certain versions of this illusion, a wave is perceived. Heeger et al show that the perception is a wave across the cortex



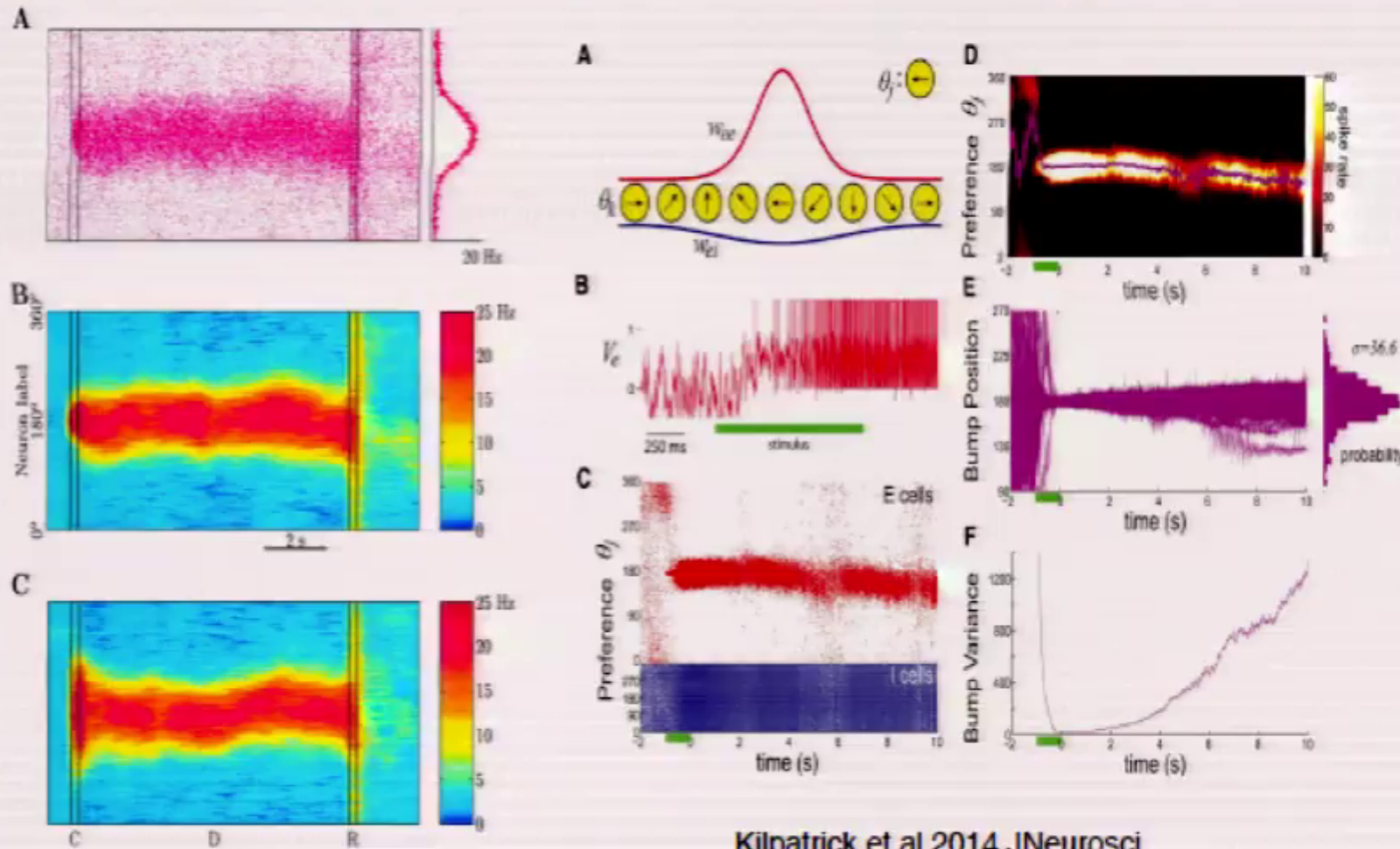
# CONTROL OF LIMBS

Heitmann et al have shown that by using anisotropic dendritic fields, they can control a limb with spatio-temporal motor cortex patterns



# LOCAL PATTERNS - WORKING MEMORY

Compte et al [2000] (and many others - 1977 on) suggest that working memory is encoded as a spatio-temporal attractor



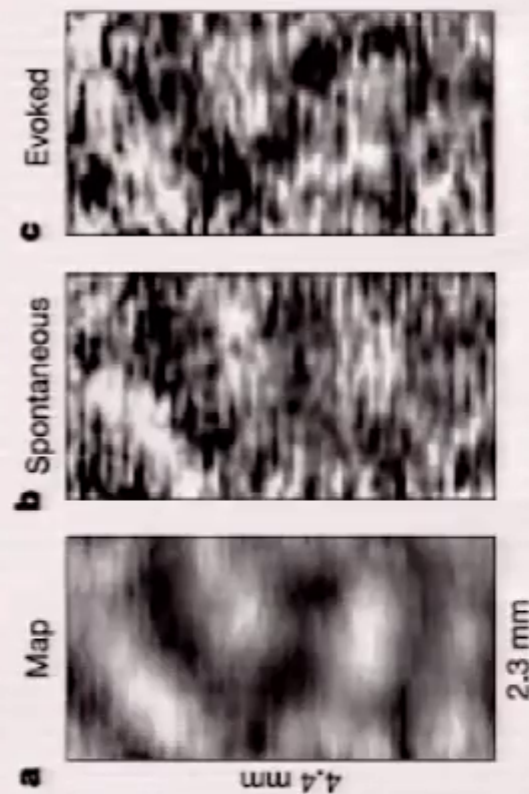
compte et al 2000 CC

Kilpatrick et al 2014 JNeurosci



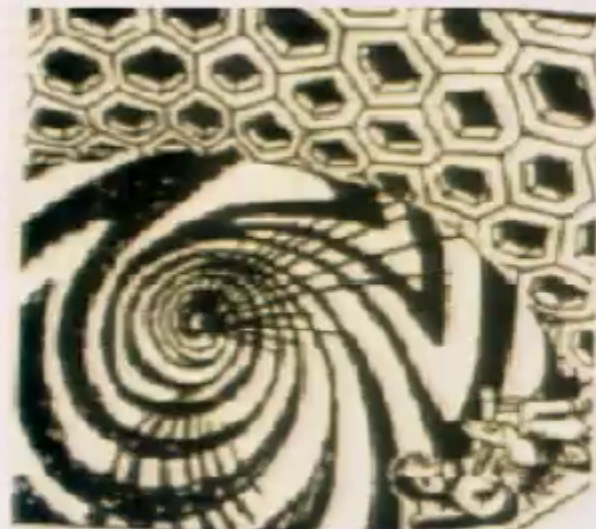
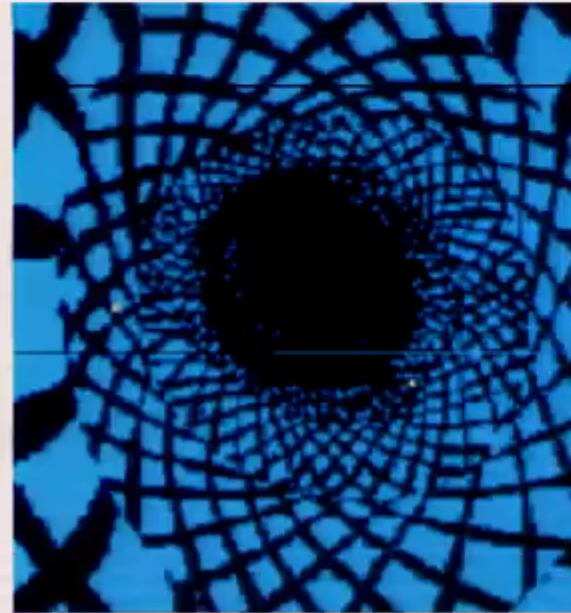
# REFLECTING EVOKED ACTIVITY

Tsodyks lab (Kenet et al, 2003) showed the ongoing activity in visual cortex was similar to that evoked by oriented bars



## VISUAL HALLUCINATIONS

BE, & Cowan (1979)  
suggested simple  
visual hallucinations  
were a consequence of  
instability in the early  
areas of visual  
processing

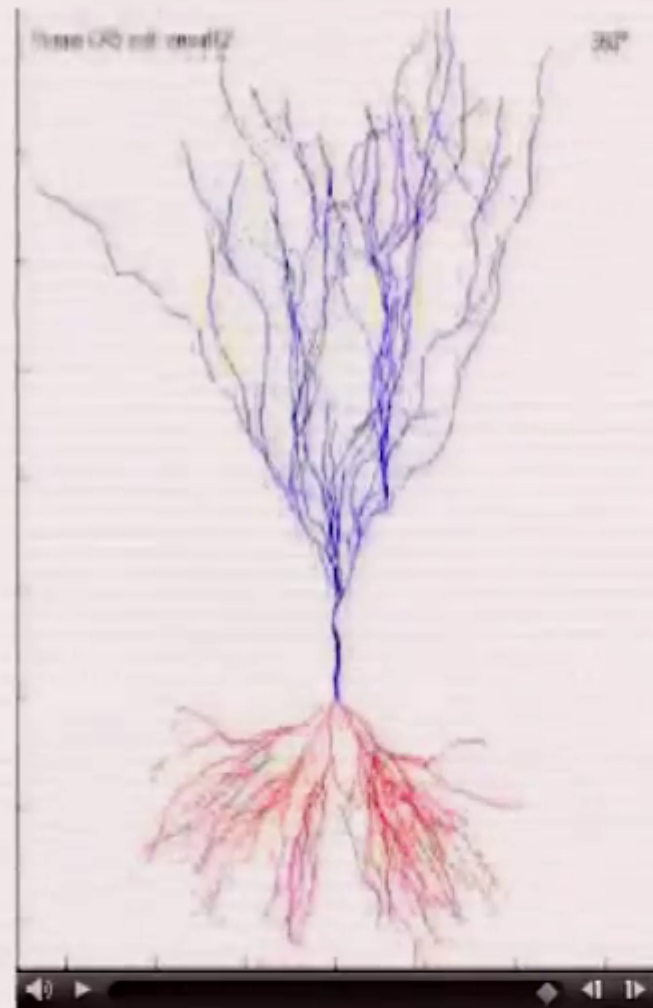




# LEVELS OF MODELING

## Single neuron level

- Include all the dendrites & axons
- Ionic channels
- Imagine thousands of them in a network



# NETWORKS OF SIMPLER MODELS

- Instead of full blown compartments & channels, each neuron is modeled as a one-dimensional (discontinuous) ODE

$$\frac{dV}{dt} = f(V, I)$$

- Networks become:

$$\frac{dV_i}{dt} = f_i(V_i, I_i)$$

$$I_i = I_i^{stim}(t) + \sum_j g_{ij} s_{ij}(t)$$

$$\tau_{ij} \frac{ds_{ij}}{dt} = -s_{ij} + \delta(t - t_i^{spike})$$

- Still hard to analyze, especially in spatial networks

# CERTAIN REDUCTIONS ARE POSSIBLE

- It is possible to make a principle reduction of “spiking models” to a *mean field* (see Brunel, et al) but this only works in steady state
- Averaging methods (slow synapses) can be used, especially for the 1-d simpler models (slow scale is synapse)
- Weak coupling and near bifurcations (BE, Izhikevich, etc)
- Equation-free modeling
- **Can also develop heuristic neural fields models.**



QUICK EXAMPLE OF AVERAGING - GOTTA BE AN  $\epsilon$ 

- Fast system depends on slow synapses

$$C \frac{dv_i}{dt} = I_{ion}(v_i, w_i) + \sum_j [g_{ij} s_j] (V_R - V_i)$$

- Say, for fixed  $\{s_j\}$  oscillation with frequency  $F_i(\{s_j\})$
- *Slow* synapse obeys

$$\frac{ds_i}{dt} = \epsilon(-s_i + \delta(v_i - V_T))$$

- Apply averaging to reduce to

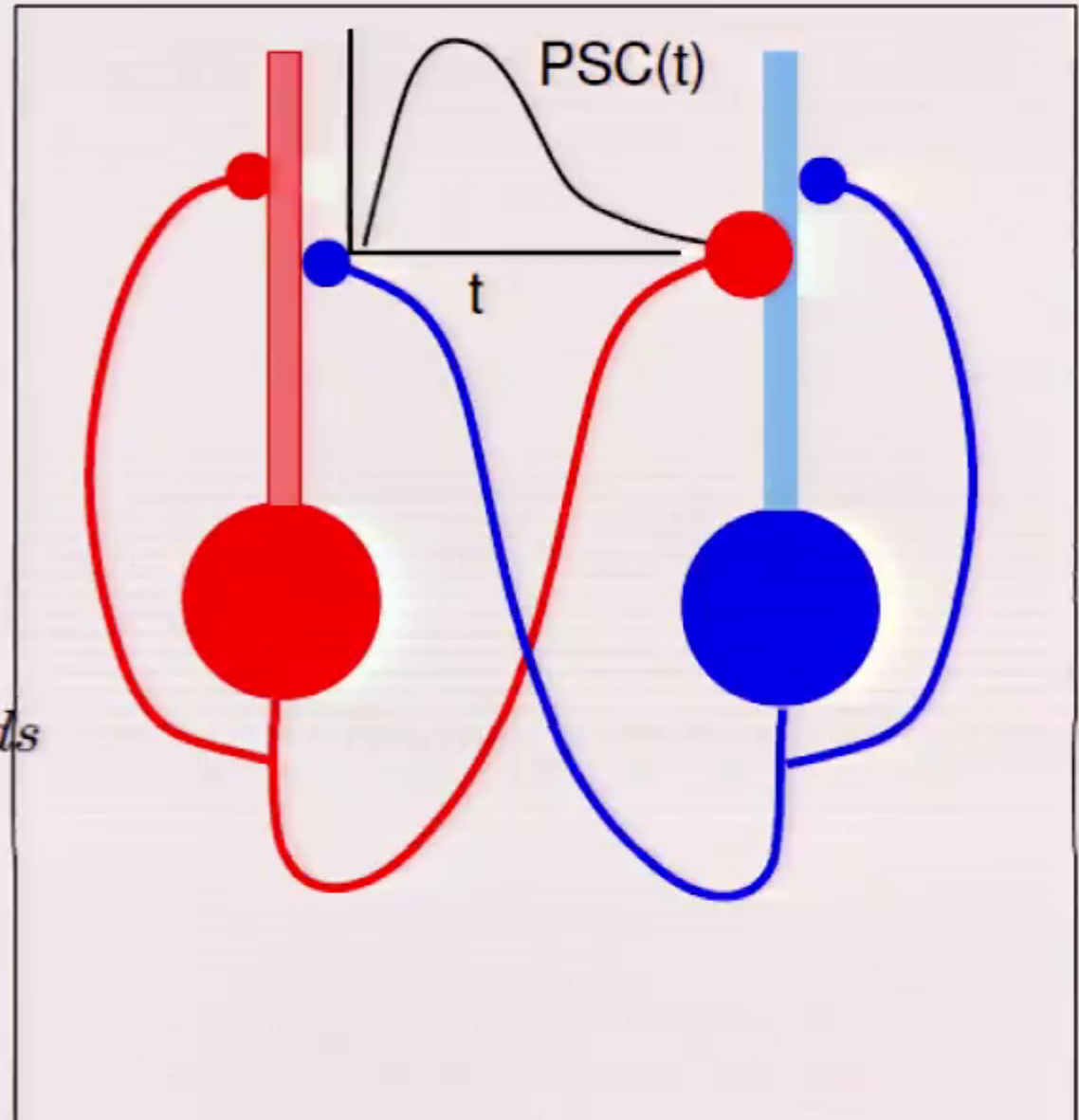
$$\frac{ds_i}{dt} = \epsilon[-s_i + F_i(\{s_j\})]$$



# FIRING RATE MODELS

inducing transmitter  
release and a  
post-synaptic current  
(PSC)

$$PSC(t) = \int^t k_s(t-s) f_e(s) ds$$

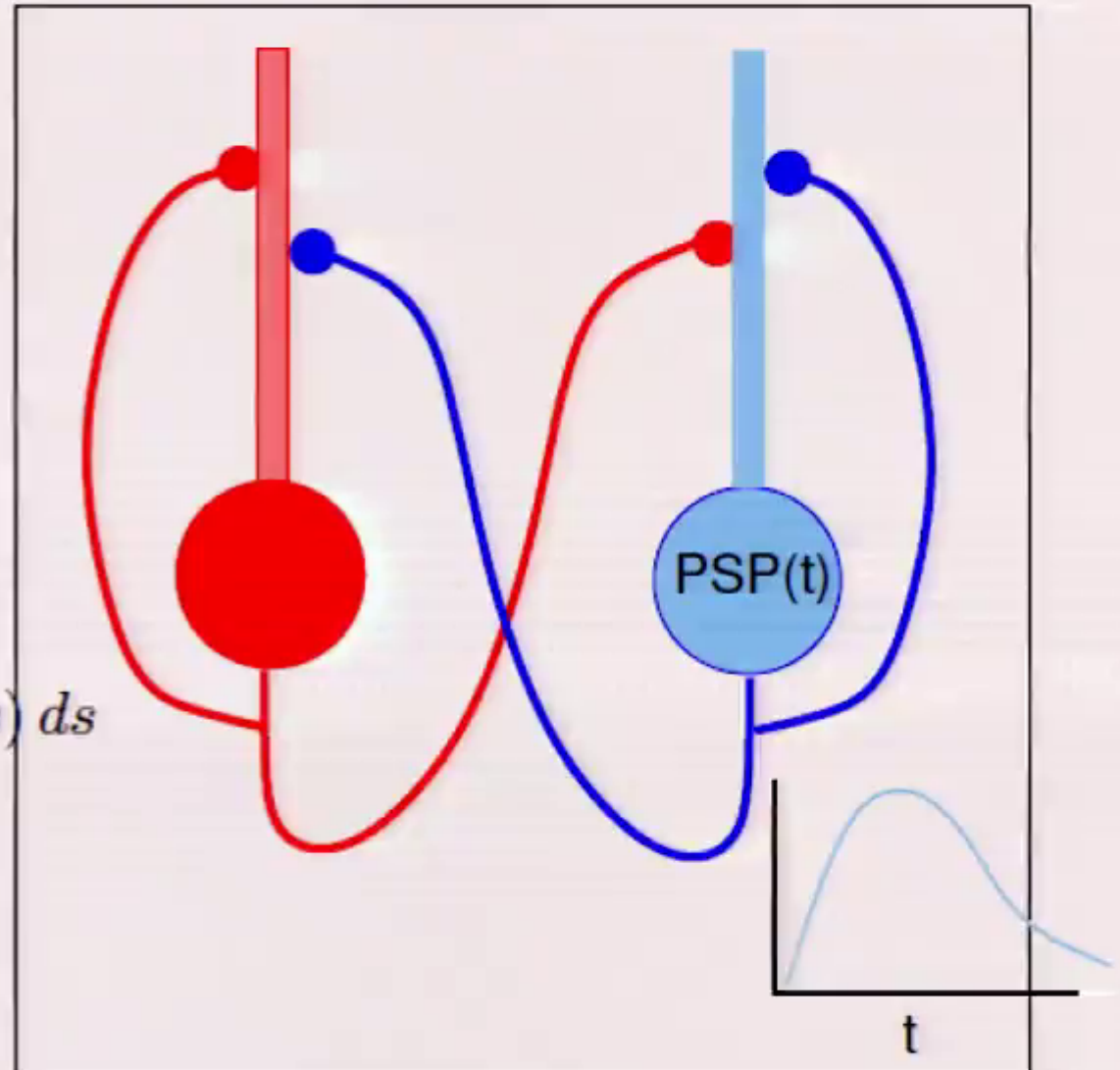




# FIRING RATE MODELS

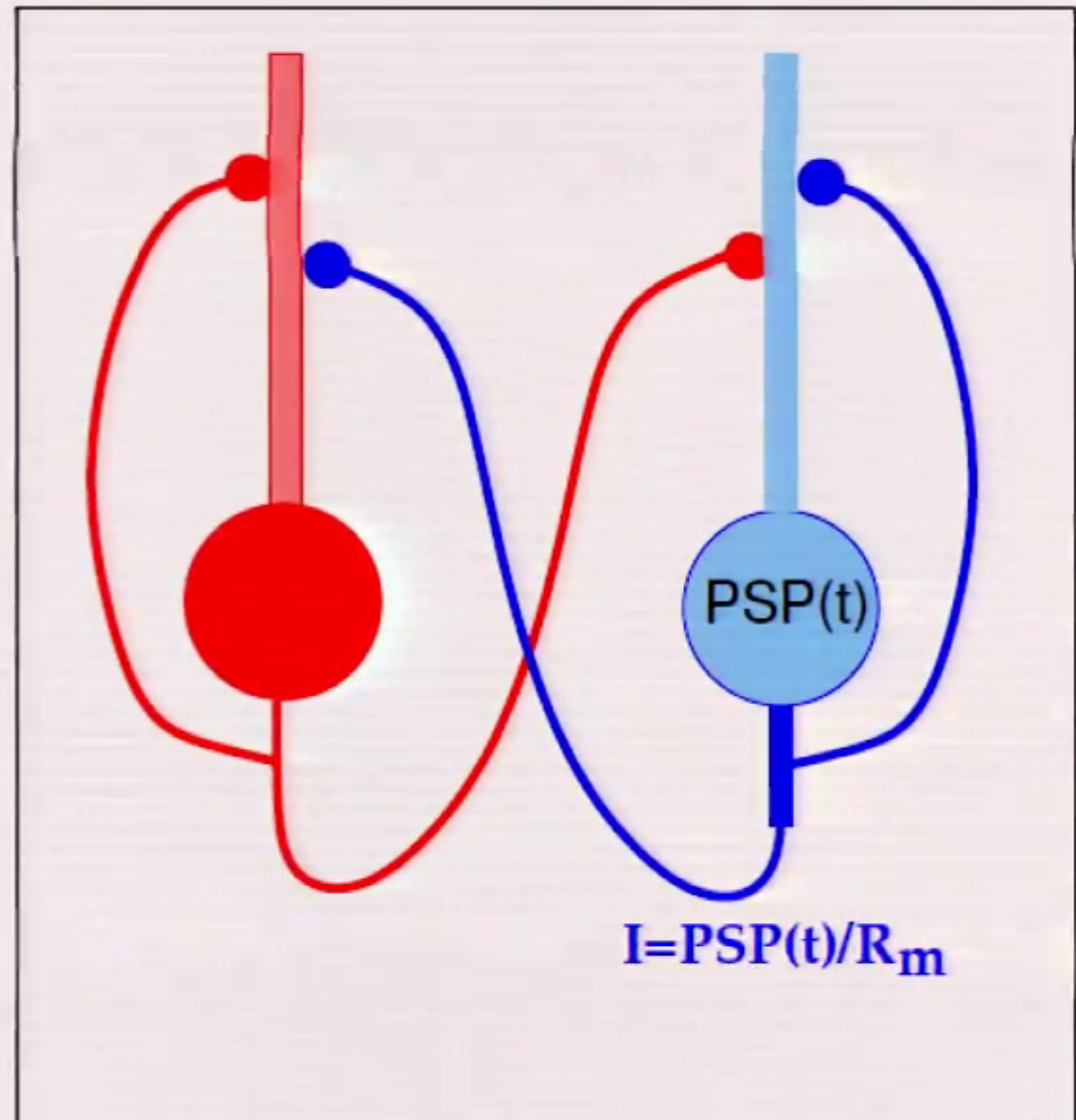
This is filtered through the dendrites for a post synaptic potential (PSP)

$$\text{PSP}(t) = \int^t k_d(t-s)\text{PSC}(s) ds$$



# FIRING RATE MODELS

and becomes the  
current at the hillock,  
closing the system



## SPACE CLAMPED MODELS

$$f_i(t) = F_i[I_i(t) + g_{ij} \sum_j k_d^i(t) \otimes k_s^j(t) \otimes f_j(t)]$$

- $F_i[\cdot]$  is the firing rate
- $I_i(t)$  is input currents
- $g_{ij}$  is strength and sign of coupling
- $a(t) \otimes b(t)$  is temporal convolution
- $k_s^j(t)$  is synaptic profile
- $k_d^i(t)$  is dendritic filter
- Nonlinear Volterra equation!

# TWO SIMPLIFICATIONS

- Instant dendritic response and exponential synapses.  
Temporal response profile depends on the **sender**

$$\tau_{s,i} \frac{du_i}{dt} = -u_i + F_i \left[ I_i + \sum_j g_{ij} u_j \right]$$

- Instant synapses and exponential dendrites. Temporal response profile depends on the **receiver**

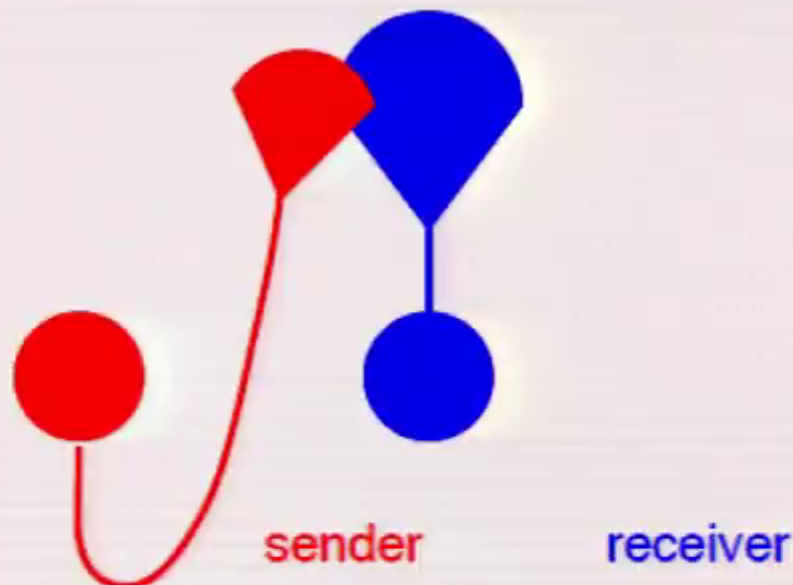
$$\tau_{m,i} \frac{dV_i}{dt} = -V_i + I_i(t) + \sum_j g_{ij} F_j(V_j)$$





# WHAT ABOUT SPACE?

Spatial interactions depend on the combined interactions between the **sender (axonal)** spread and the **receiver (dendritic)** spread



$$W(x) = J_a(x) \star J_d(x)$$

## THE FINAL MODEL (FOR NOW)

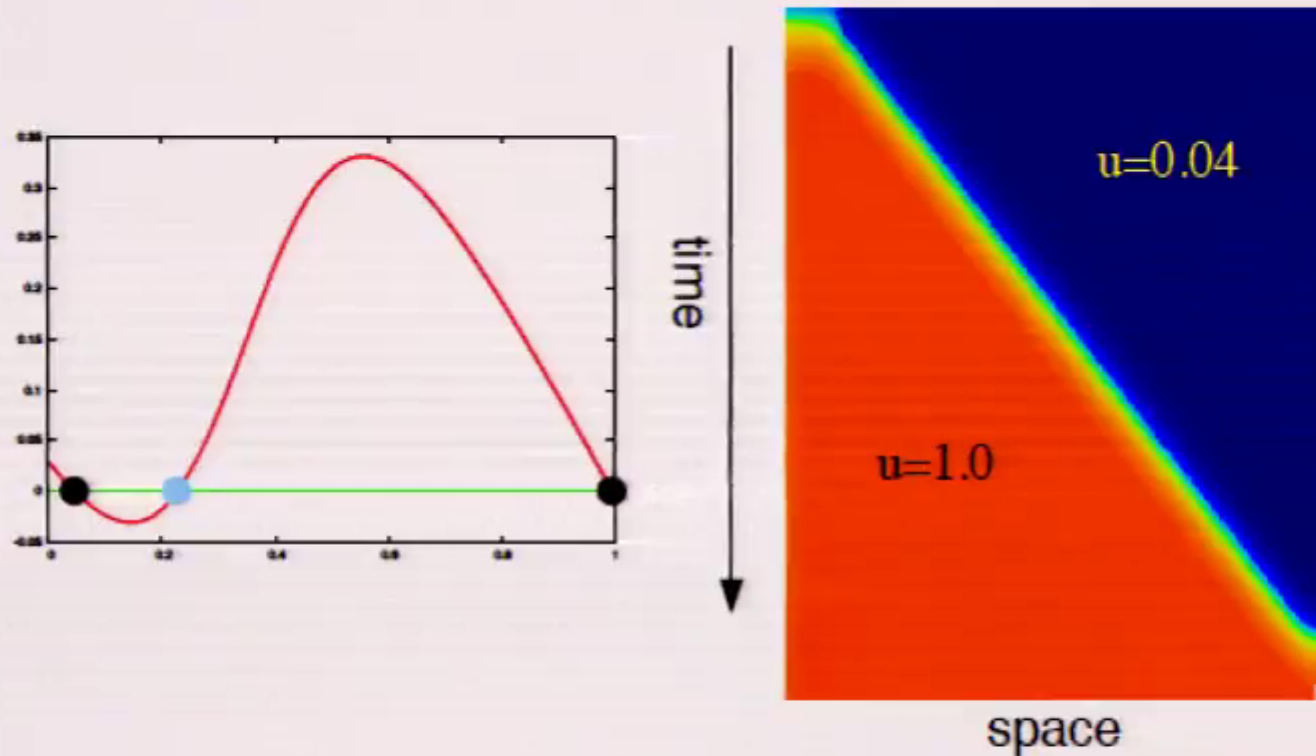
For consistency, we assume the interaction depends only on the **sender(axon)**

$$\begin{aligned}\tau_e \frac{\partial u}{\partial t} &= -u + F_e [g_{ee} W_e(x) \star u - g_{ei} W_i(x) \star v + I_e] \\ \tau_i \frac{\partial v}{\partial t} &= -v + F_i [g_{ie} W_e(x) \star u - g_{ii} W_i(x) \star v + I_i]\end{aligned}$$

The  $\star$  is convolution in space (1- or 2-D)



## THE SIMPLEST – THE SCALAR WAVE FRONT



$$\frac{\partial u}{\partial t} = -u + F[J_{ee}(x) \star u]$$

## EXISTENCE STRATEGY (BE &amp; B. MCLEOD)

- Traveling wave:

$$c\tau_e u' = -u + F[J_{ee} \star u]$$

- Nonlocal equation needs to be localized
- If  $J_{ee}(x) = g_{ee}e^{-|x|}/2$  then invertible

$$\begin{aligned} c\tau_e u' &= -u + F[g_{ee}z] \\ z'' &= z - u \end{aligned}$$

- Use homotopy to go from restricted model (shooting!) to true model



# A CLASS OF SOLVABLE MODELS

- If we replace  $F(x)$  with  $\text{heav}(x - \theta)$ , the step function, then we can construct solutions
- E.g for the exponential,

$$c = \frac{1}{\tau_e} \frac{1 - 2\theta}{2\theta}$$

- Formal stability can also be determined
- Many other solvable problems

# TRAVELING PULSES

- Fronts are fairly unusual (except see below); what is more common are pulses

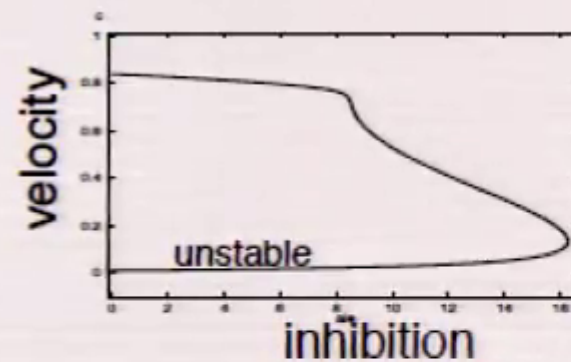
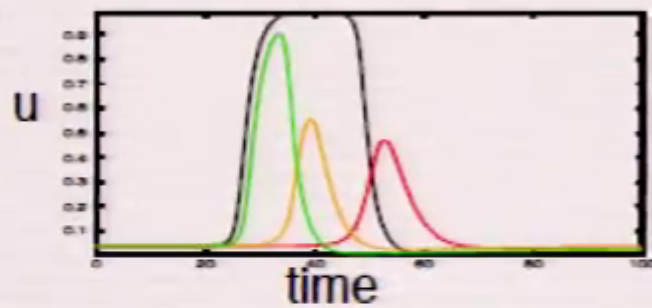
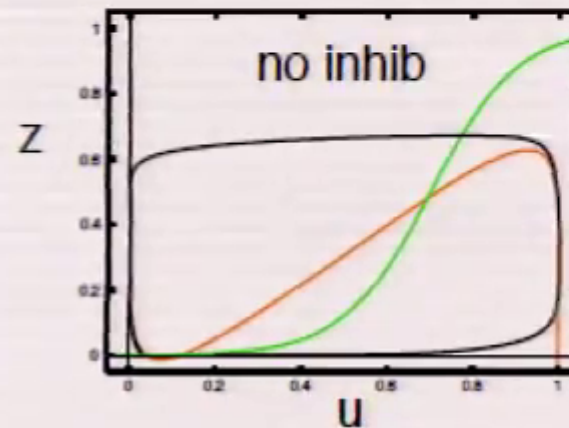
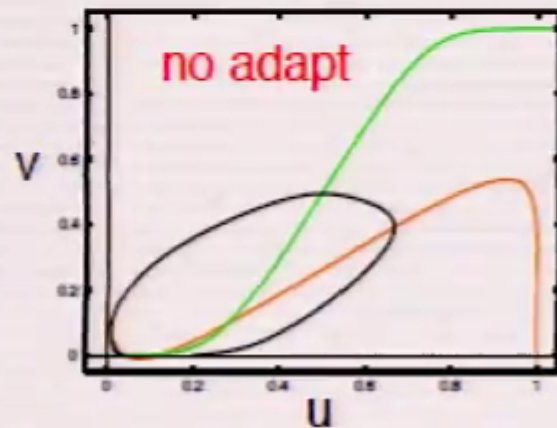
# TRAVELING PULSES

- Fronts are fairly unusual (except see below); what is more common are pulses
- Many experiments going back to the 80's on *disinhibited slice*
  - Golomb-Amitai model conductance based adds *adaptation* that brings activity back down
  - Pinto-Ermentrout model constructs pulses using existence of fronts and singular perturbation

$$\begin{aligned}V_t &= -V + J_e(x) \star F[V] - Z \\Z_t &= \epsilon[-Z + \alpha V]\end{aligned}$$

- Hastings recently has some existence results for nonlinear adaptation
- **What about intact inhibition?**

# ADAPTATION PLUS INHIBITION

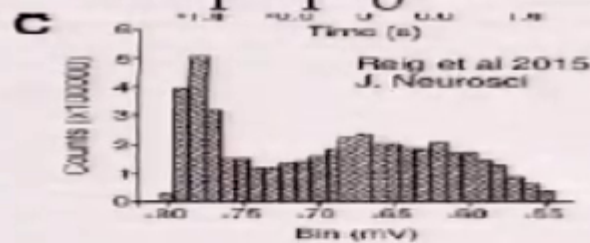


$$\begin{aligned} \tau_e u' &= -u + f_e(\dots - a_{ez}z) & \tau_i v' &= -v + f_i(a_{ie}u - \dots) \\ \tau_z z' &= -z + f(a_{ze}u - \theta_z) \end{aligned}$$



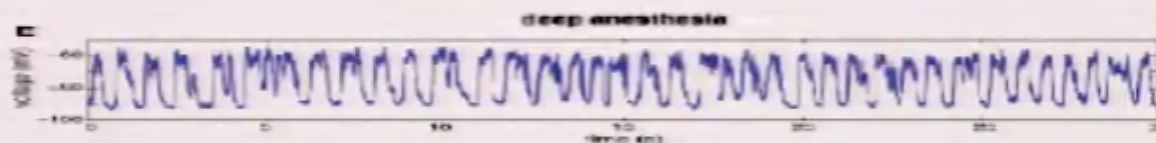
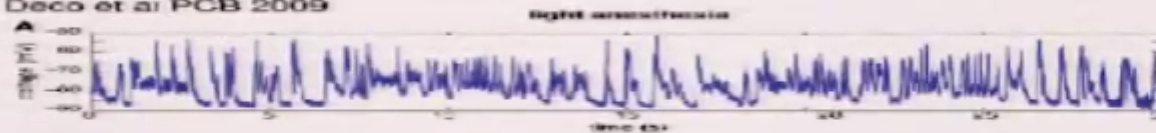
## UP/DOWN STATES

- Switch down to up and vice versa with same stimulus
- UP propagates
- Strong stimuli only transiently UP
- Larger variance in UP



Variance UP > Variance DN  
Less Rhythmic during light anesthesia

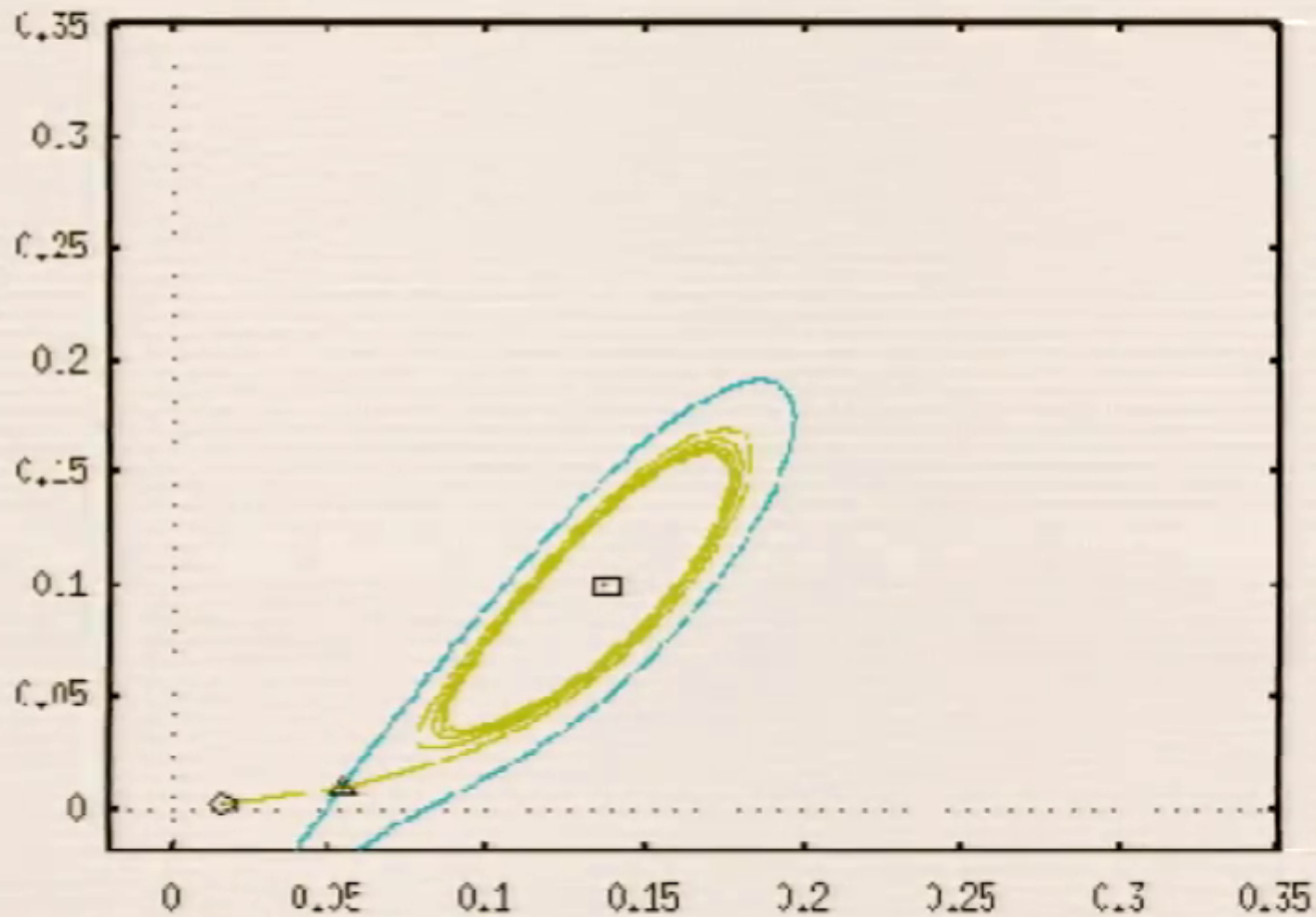
Deco et al PCB 2009



## SUGGESTING A PHASE-PLANE

 $t_{cut} = 2.5$ 

V vs U

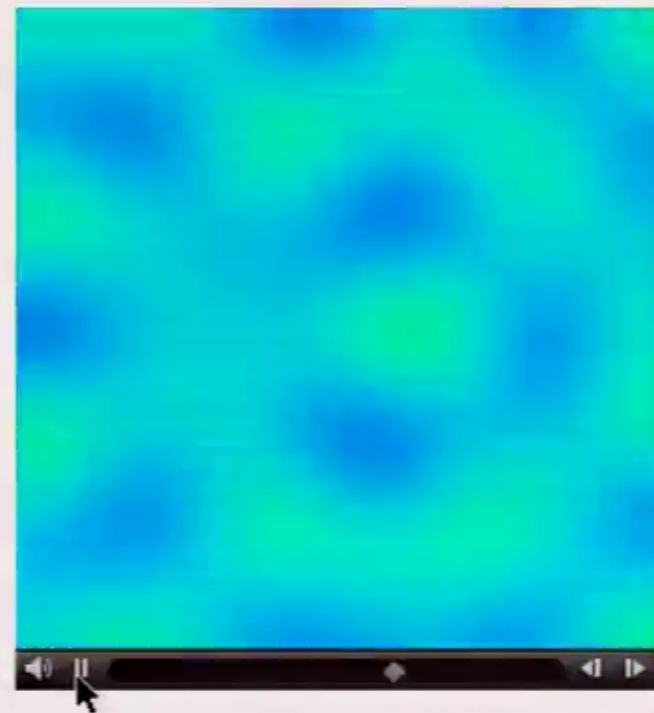


## ADVERTISEMENT

- For small  $\tau_i$  can get waves from DOWN to UP
- As  $\tau_i$  increases, lose the UP attractor and revert to excitable
- When  $f_{e,i}$  are step functions, very cool Filippov system with sliding, grazing, etc
- See MS 87 tomorrow!

## PATTERNS WITH NO MEXICAN HAT

- Aghajanian has shown that 5HT (related to effects of LSD) puts neurons to up state
- If the up state is near a homoclinic LC, then can detabilize homogenize state *even when spread of E exceeds spread of I*





# ROTATING/SPIRAL WAVES

- The local dynamics is either excitable or oscillatory
- Such as in the previous model for traveling waves in one-dimension
- With the right heterogeneities or initial data, spatial coupling can lead to rotating waves

# ROTATING WAVES

Class I (SNIC) excitability gives complex patterns



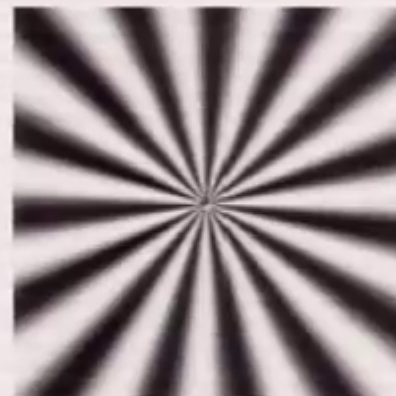
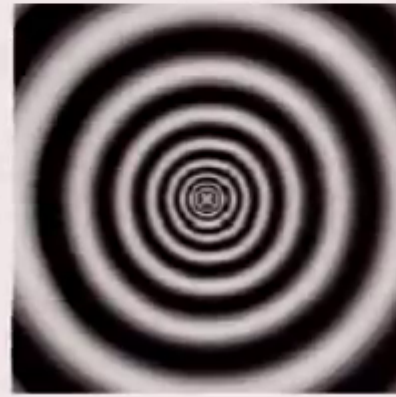
Class II (Hopf) excitability gives nice rotating waves



## ONGOING ACTIVITY PLUS STIMULI EQUALS FUN

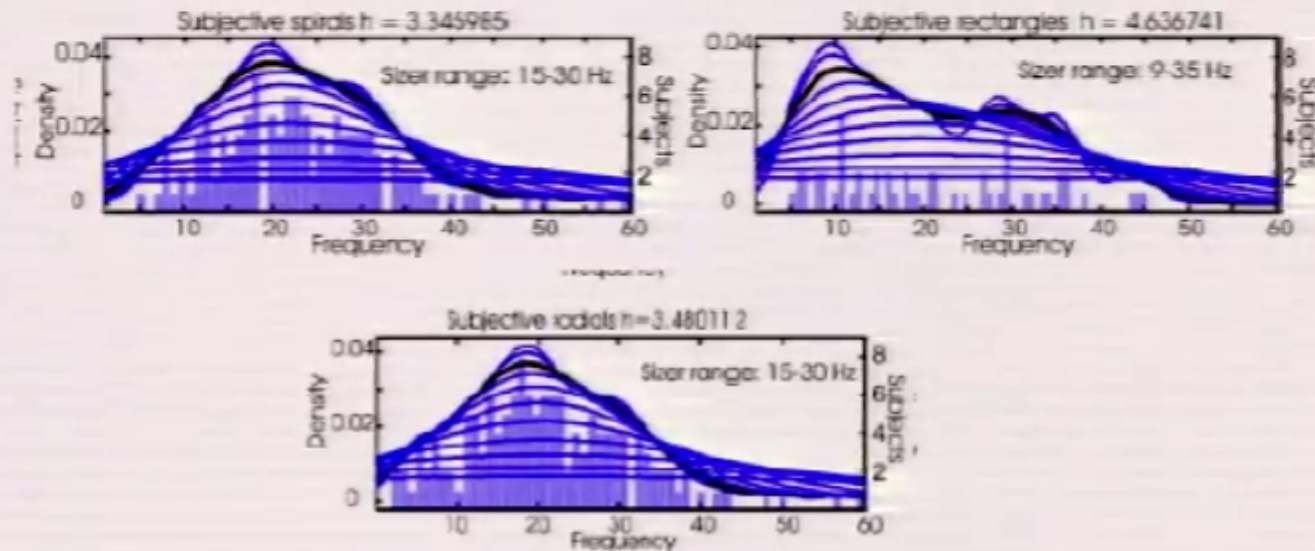
- Visual illusions can be regarded as exploiting the internal dynamics of the cortex (e.g. priors, on going activity, etc)
- Certain classes of spatially or temporally periodic stimuli can lead to complex percepts
- In pathological cases, can lead to seizures, migraines, etc (think Pokemon)
- Using the simple EI neural fields, we can provide a possible explanation

# FLICKER PHOSPHENES





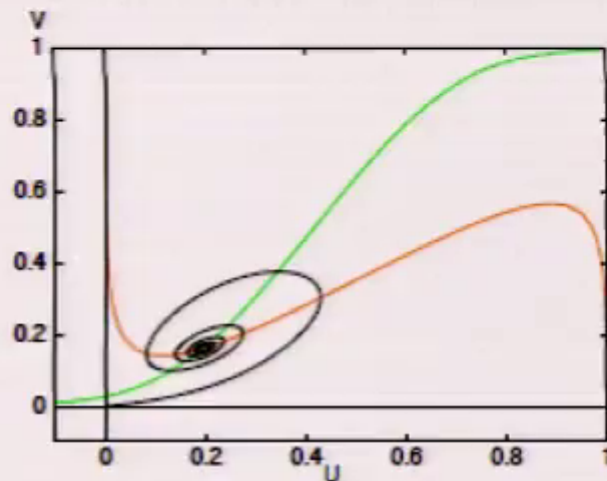
# FLICKER PHOSPHENES



*C. Becker, M.A. Ellist / Consciousness and Cognition 15 (2006) 175-196*

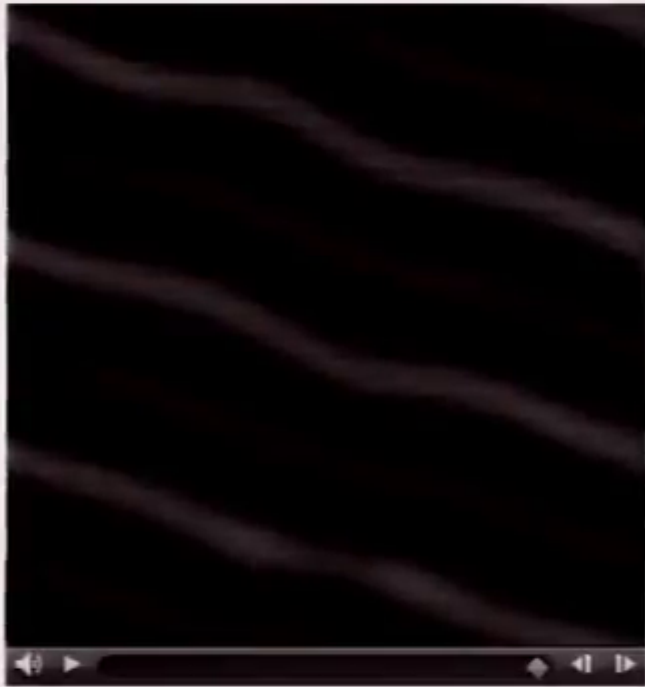
- Most prominent at 5-25 Hz uniform flicker (best binocularly)
- At low frequencies, tend to get checks/hexagons
- At high frequencies stripes

## FLICKER PHOSPHENES

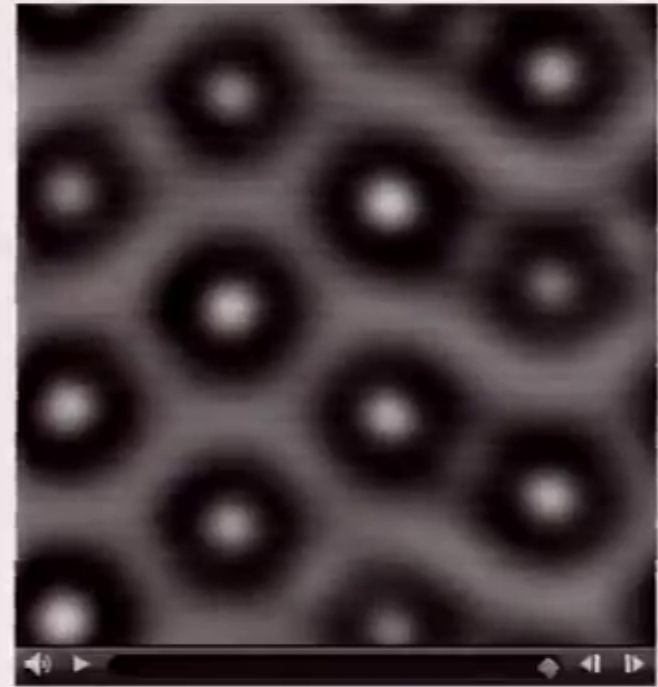


- Basic idea is to have a stable middle branch equilibrium point that has complex eigenvalues
- Oscillation timescale is related to the flicker frequency sensitivity
- Combine with spatial *lateral inhibition*

## SIMULATIONS



- At 16 Hz get stripes
- Due to period doubling symmetries
- -1 multiplier



- At 8 Hz get hexagons
- Can explain with symmetric bifurcation and Floquet theory
- +1 multiplier

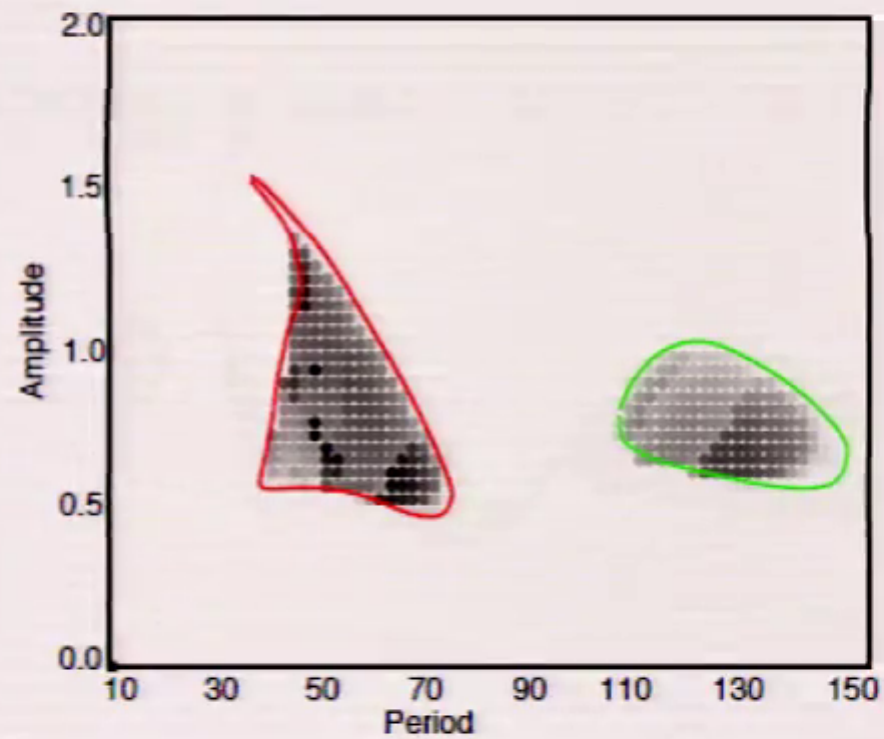
## ANALYSIS

- Solve for the spatially uniform oscillation
- Linearize and take the spatial Fourier transform
- Compute Floquet multipliers
- Use this to track the stability

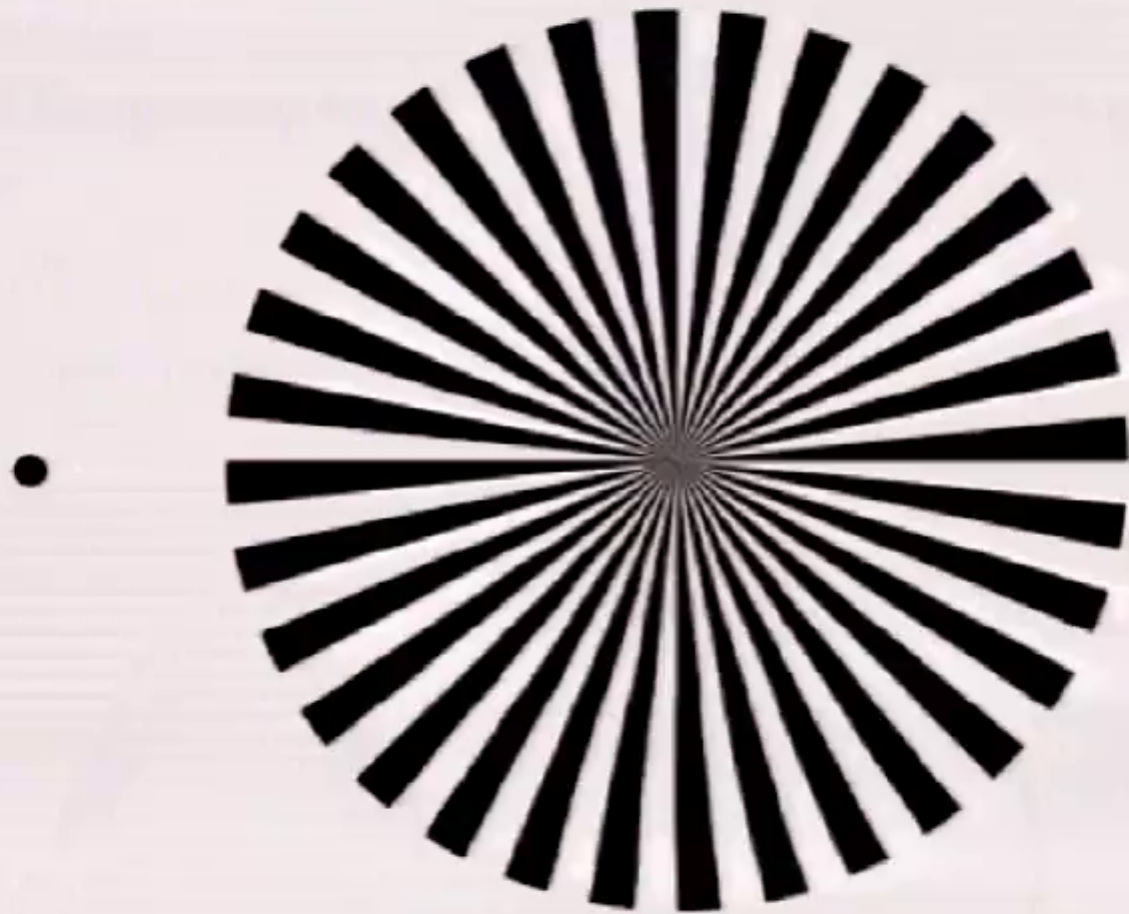




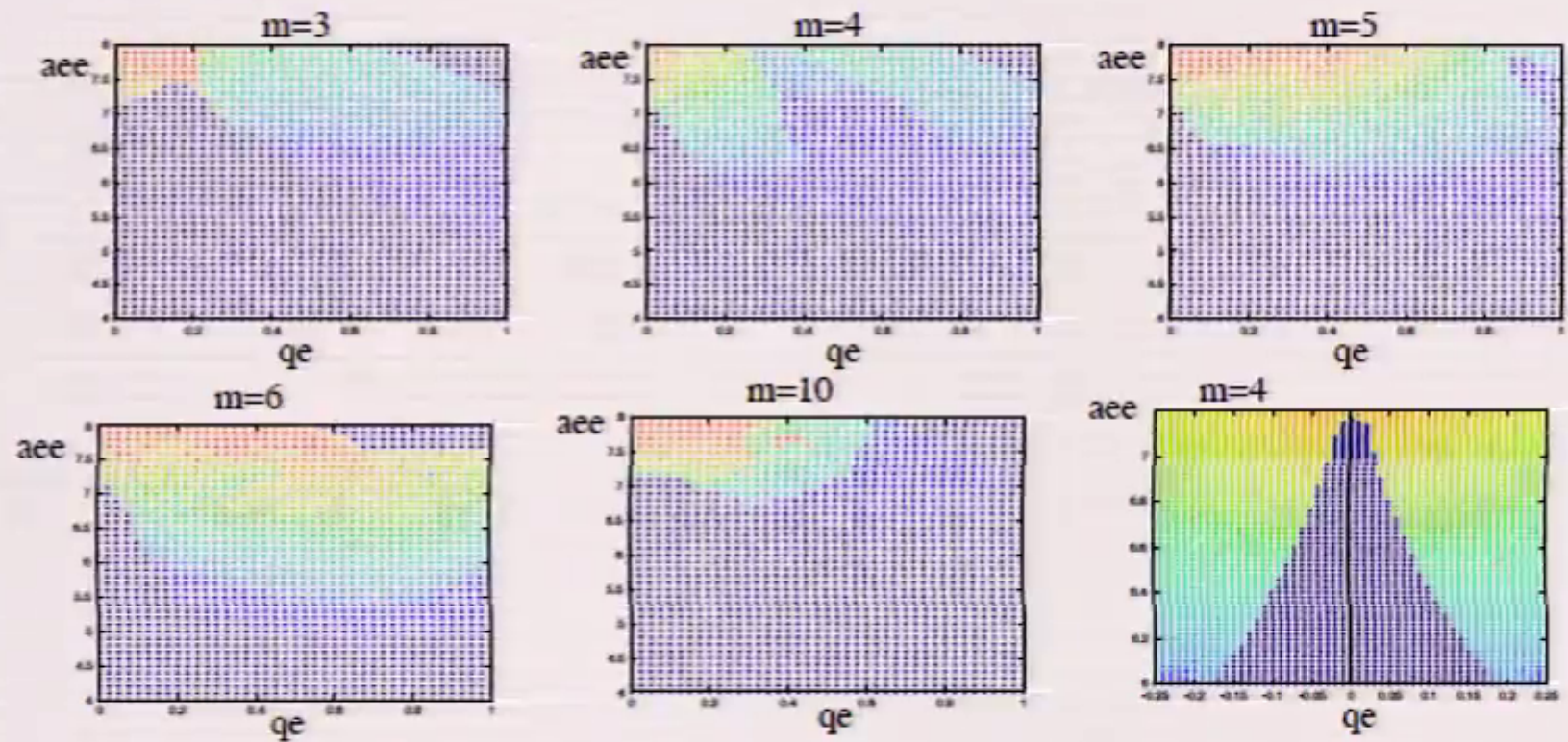
## RESULTS



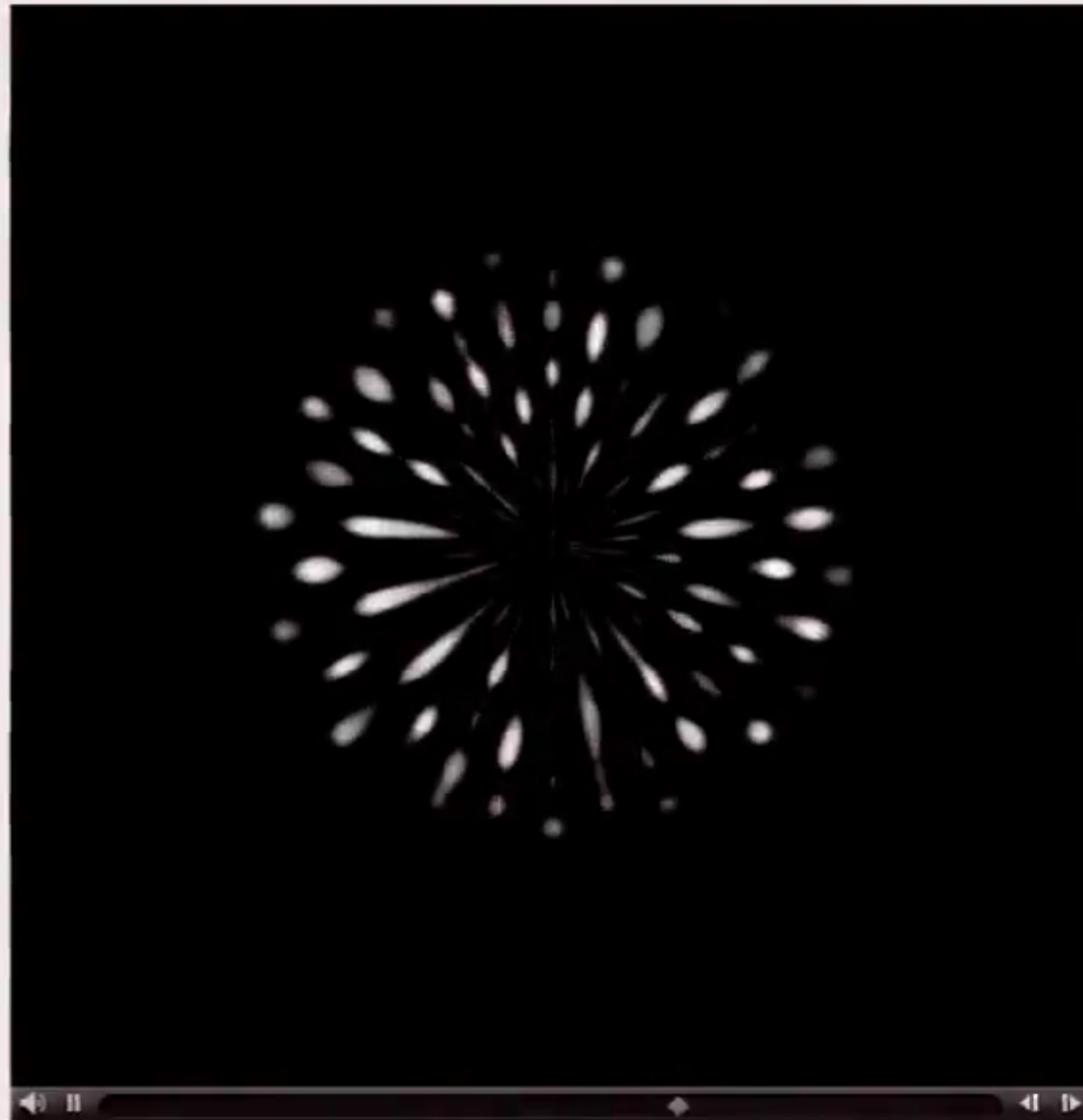
# FLICKERING PINWHEEL



# SAME MODEL - DIFFERENT STIMULUS



# AND THE PINWHEEL





# CONCLUSIONS

- With the ability of experimentalists to record at high temporal and spatial resolution, we can finally start to model and understand the role of spatio-temporal activity in cortical networks
- There are mathematical challenges related to the nonlocal interactions; stability existence, and for me, good perturbation methods
- Computational challenges related to the nonlocal interactions
  - FFT methods or inverse operator techniques
  - CUDA (GPU) computing - the B&W sims today were all done on a laptop!

# ACKNOWLEDGMENTS

## Ermentrout Lab:

- Stewart Heitmann
- Jason Pina
- Jeremy Harris
- NSF and the Benter Foundation

## Collaborators:

- Wilson Truccolo & Michael Rule
- Jian-young Wu
- Pulin Gong
- Brandon van der Ventel