

Reconstructing Rotor Dynamics from Sparse Noisy Data

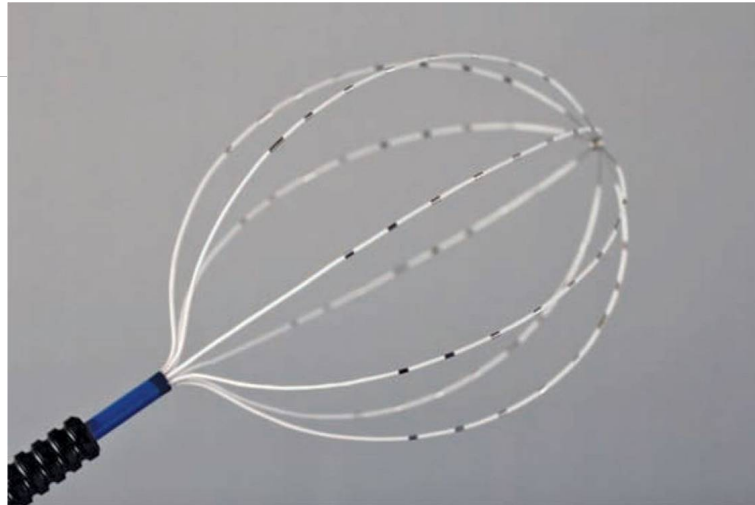
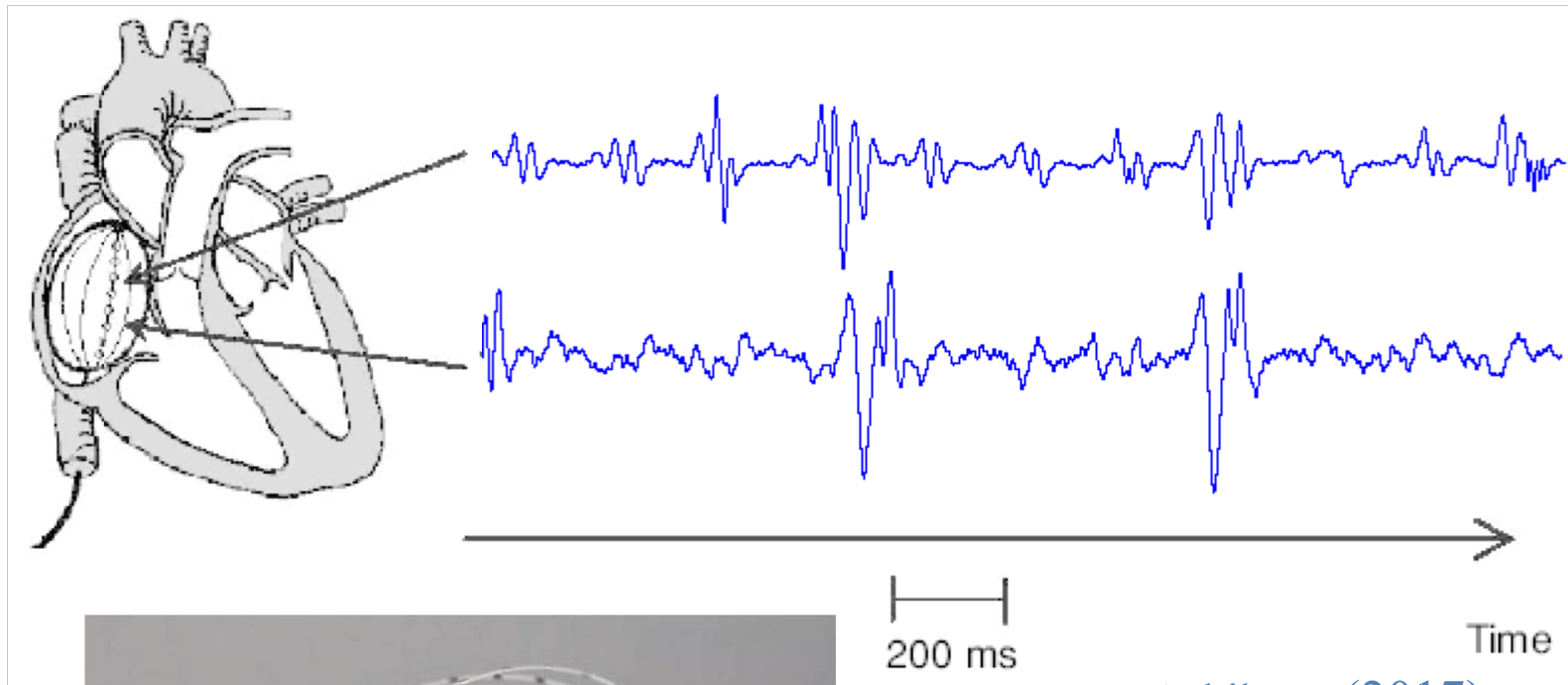
Daniel Gurevich, Roman Grigoriev



**Georgia
Tech**

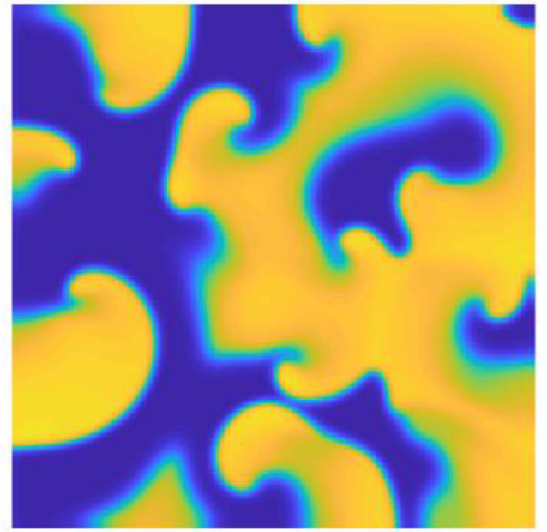


Rotor mapping for ablation therapy



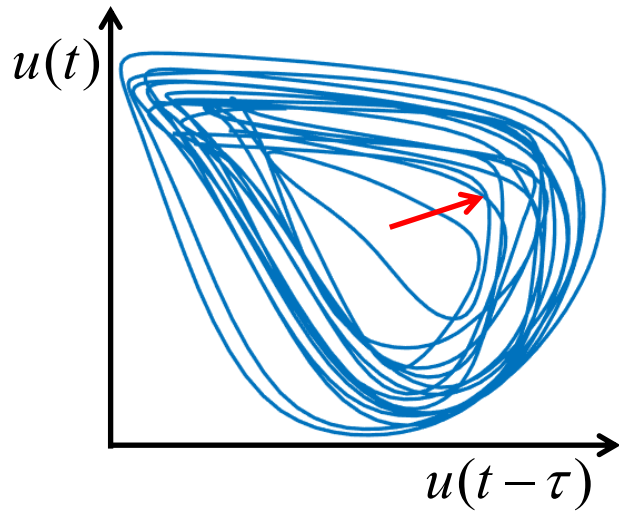
Ashikaga (2017)

Model of atrial fibrillation

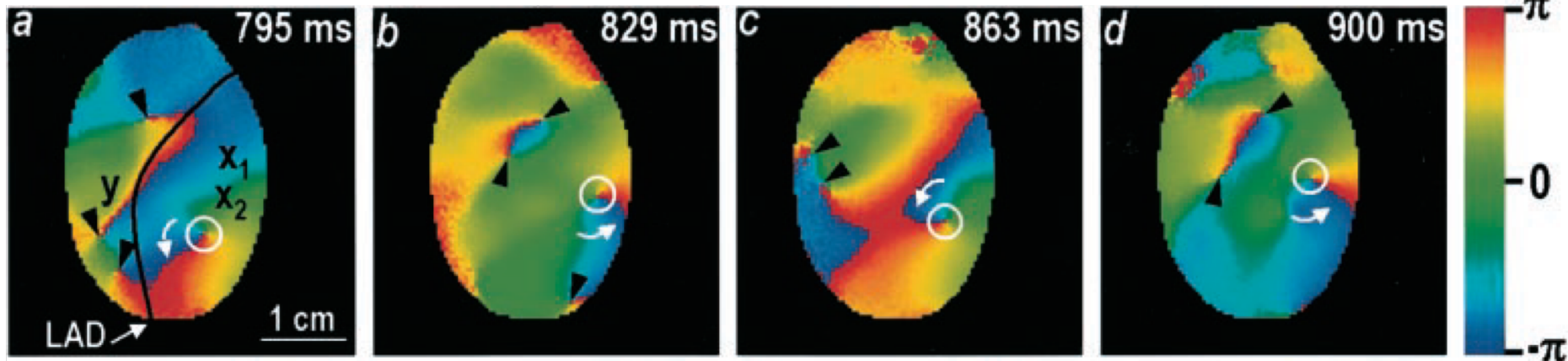


Karma model

Phase singularities

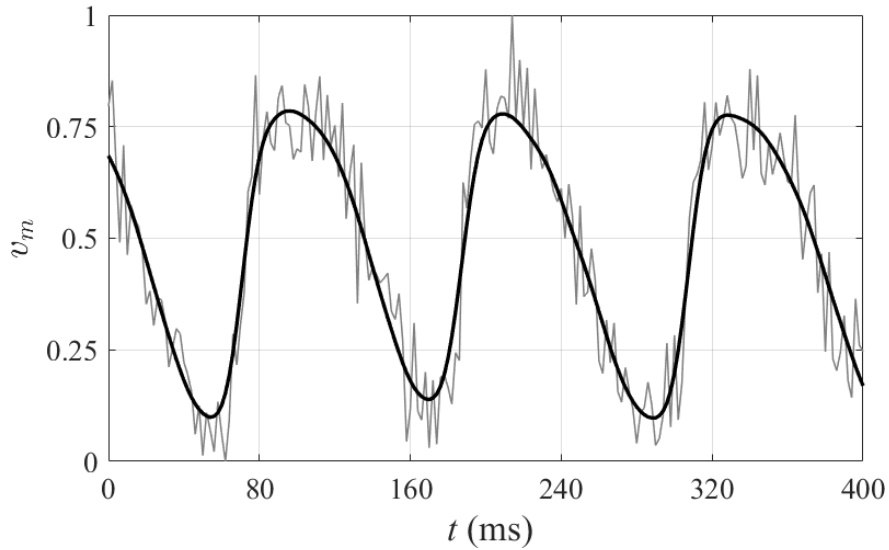


$$q = \frac{1}{2\pi} \oint d\phi = \begin{cases} -1, & \text{PS (clockwise)} \\ 0, & \text{no PS} \\ +1, & \text{PS (counter-clockwise)} \end{cases}$$

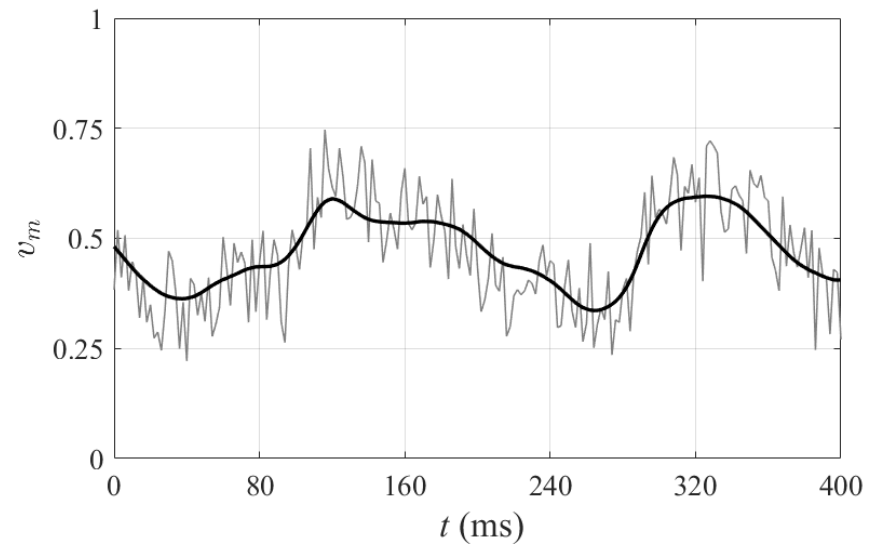


Wu et al. (2004)

Interpreting noisy data

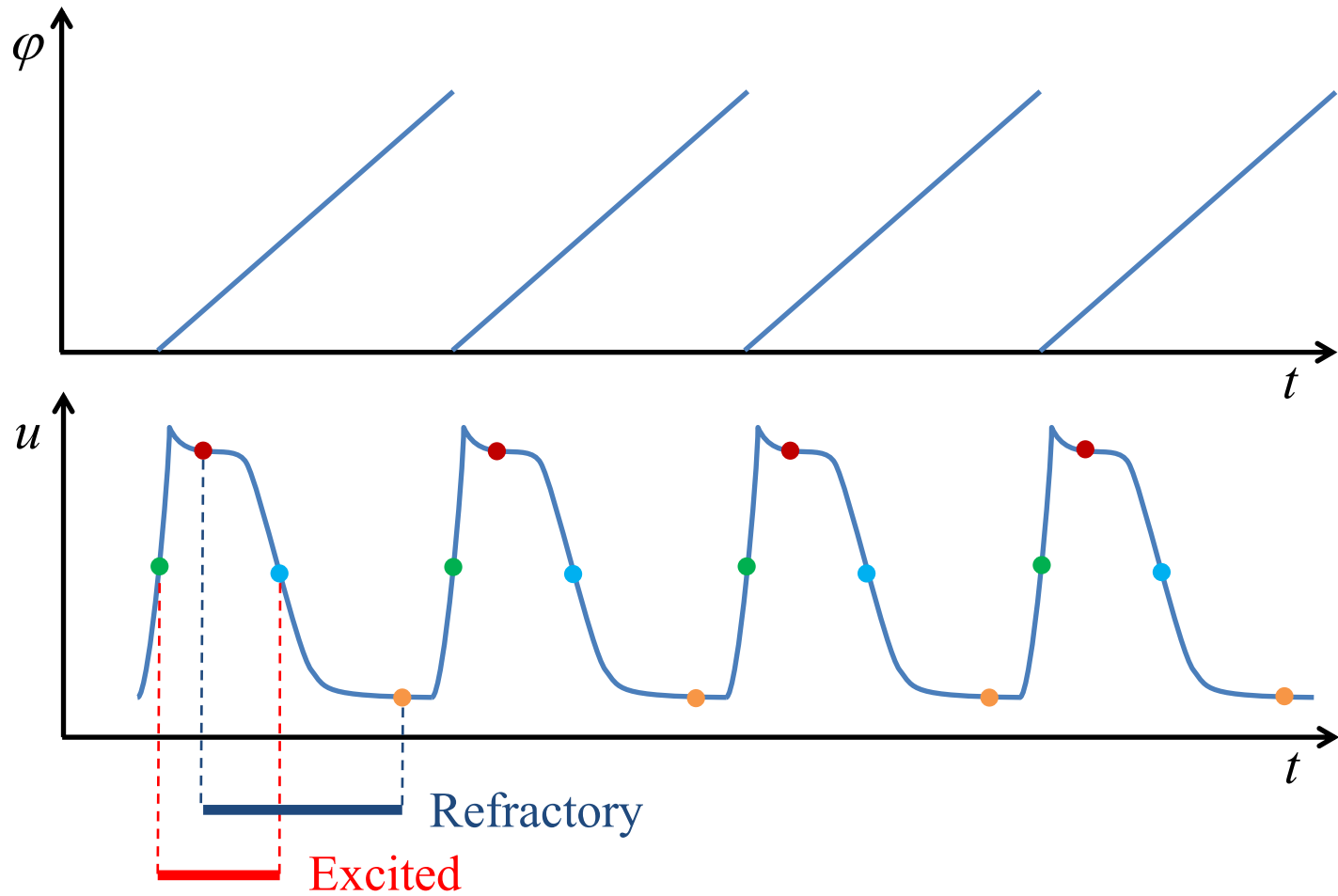


Voltage trace far from PS



Voltage trace near PS

Phase singularities & level sets

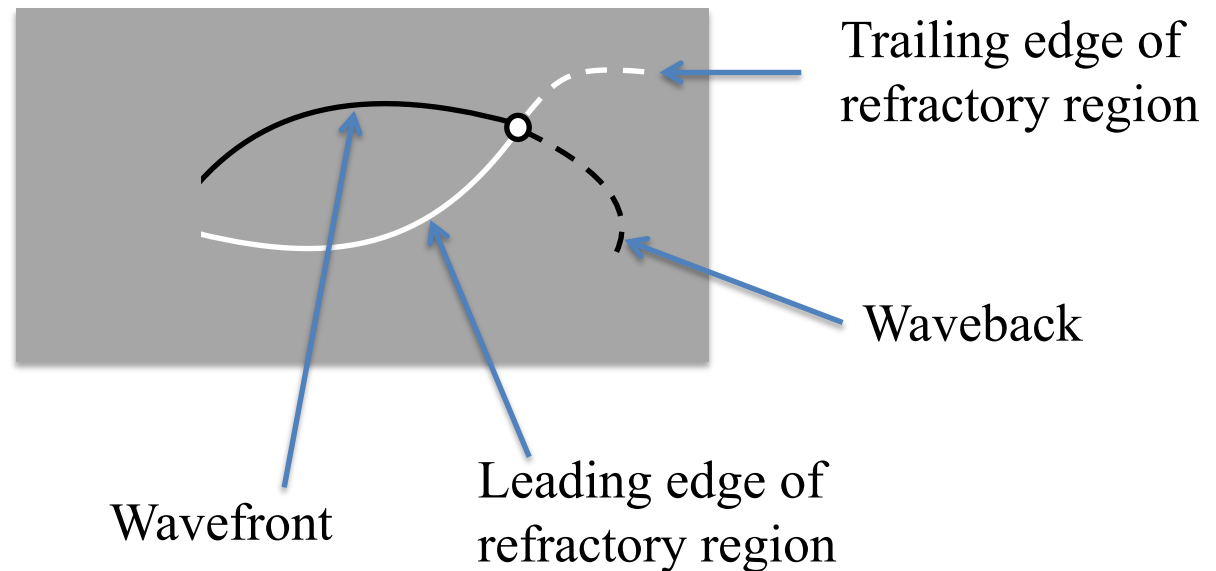


Topological description

- Complexity of the excitation pattern can be quantified by the number of phase singularities (PS)

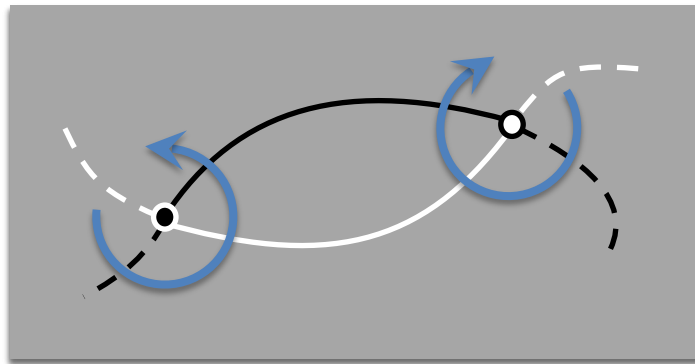
Topological description

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- Each PS lies at the intersection of two level sets (e.g., $\partial_t u = 0$ and $\partial_t^2 u = 0$).



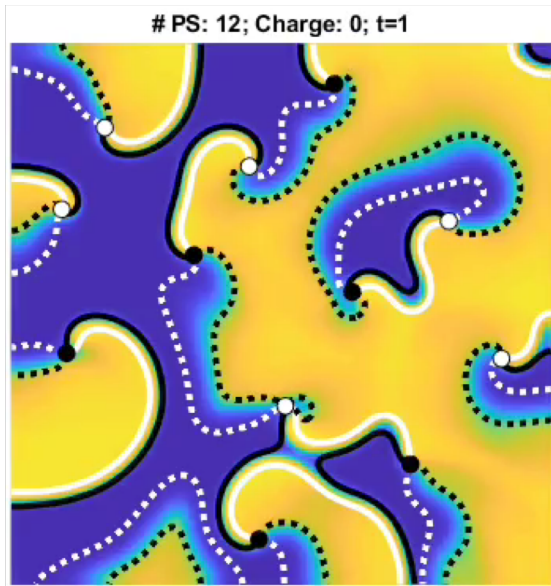
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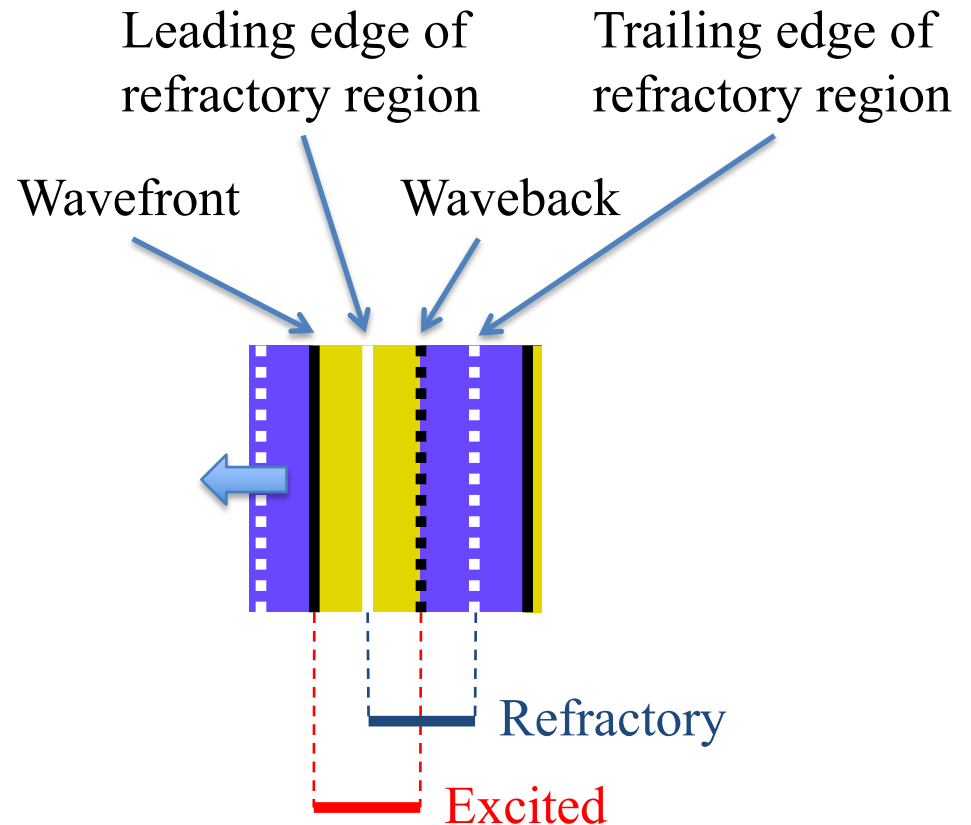


- Each PS has a topological charge: $q = \text{sign}(\hat{\mathbf{z}} \cdot \nabla u \times \nabla \partial_t u) = \pm 1$
- The net topological charge is conserved*: $\sum_i q_i = 0$
- Phase singularities can only be created/destroyed in pairs*

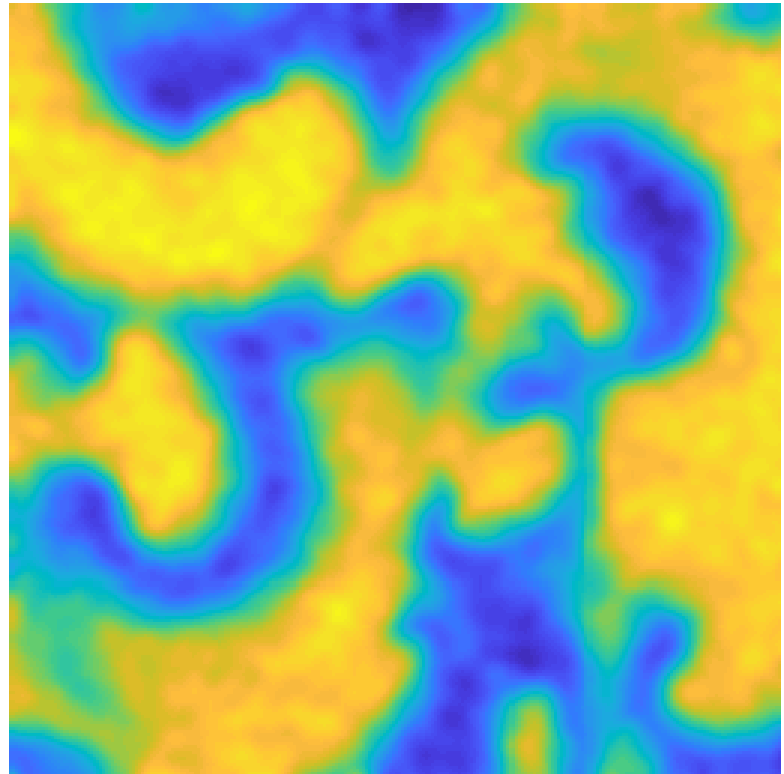
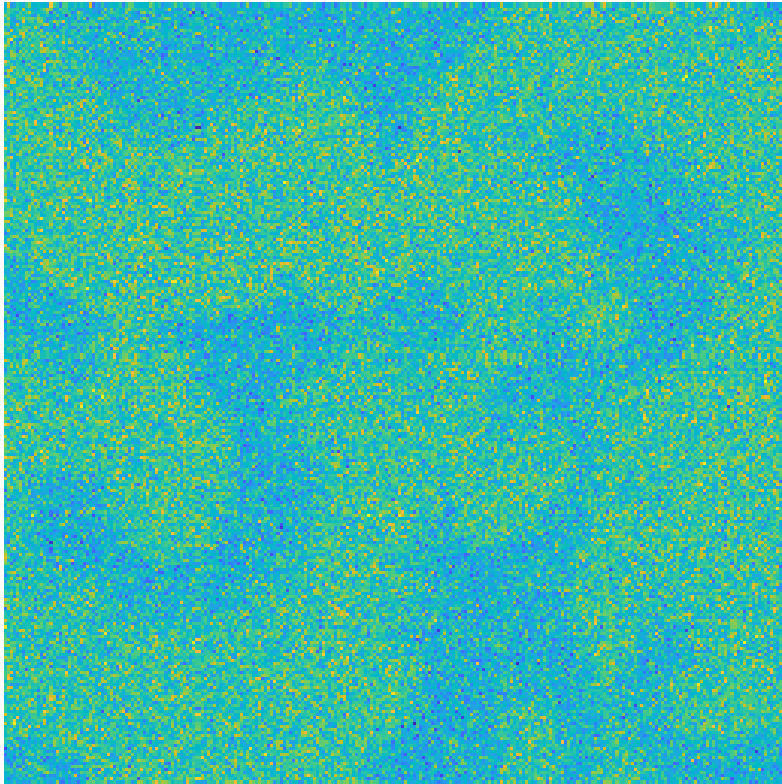
Practical implementation



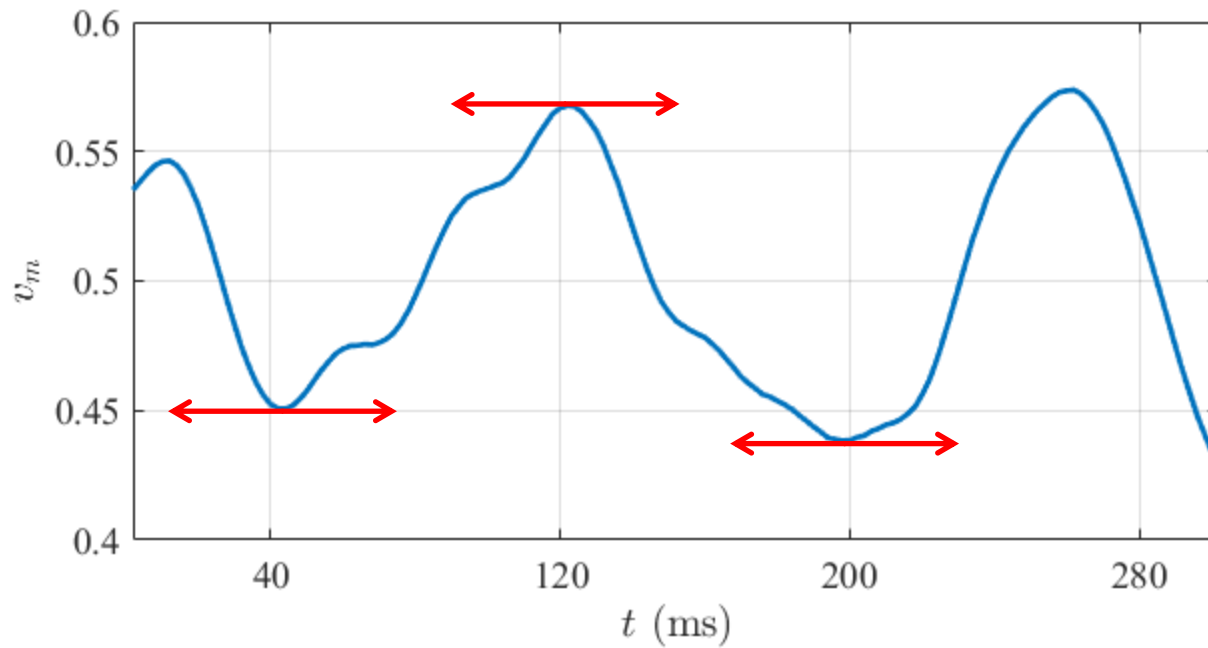
Karma model



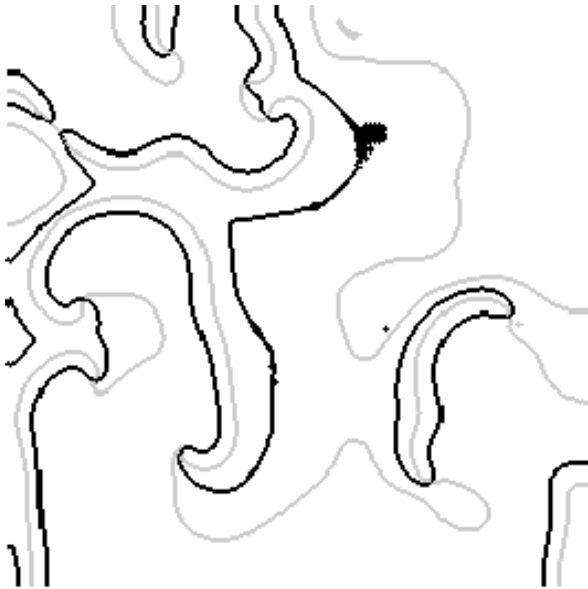
Step 1: Gaussian smoothing



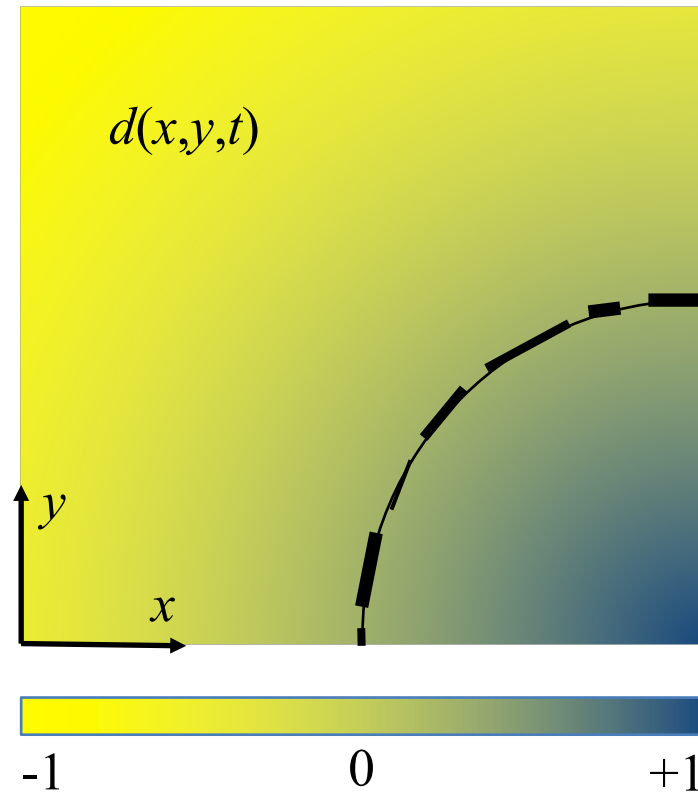
Step 2: robust “time derivative”



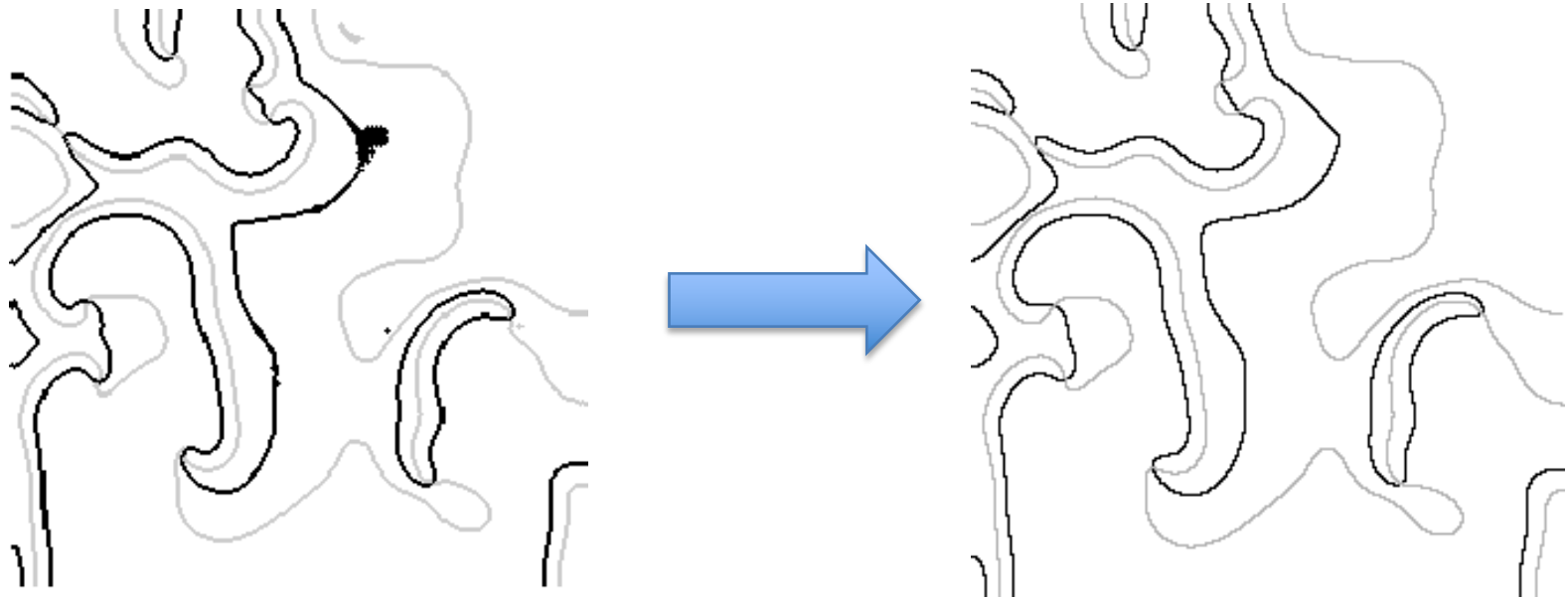
Step 3: coarse level sets



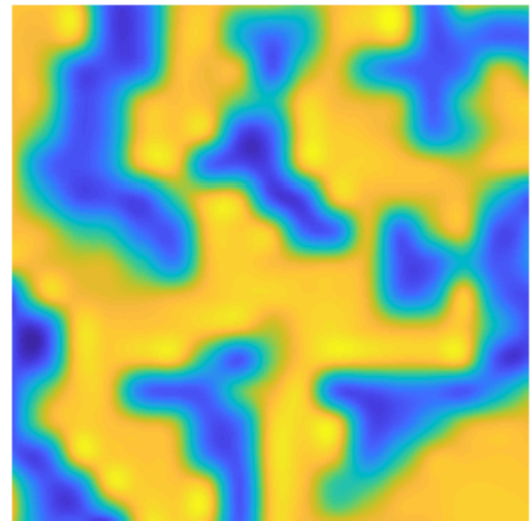
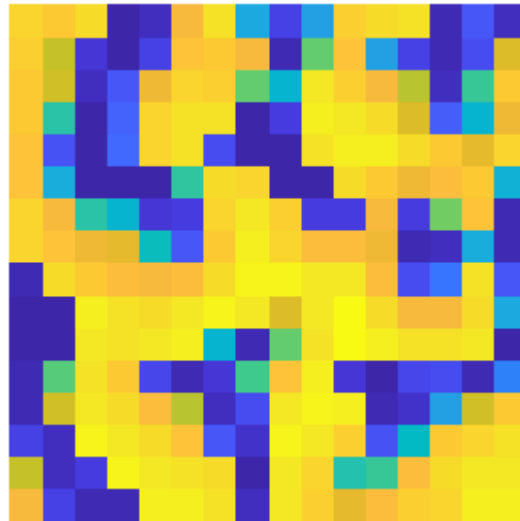
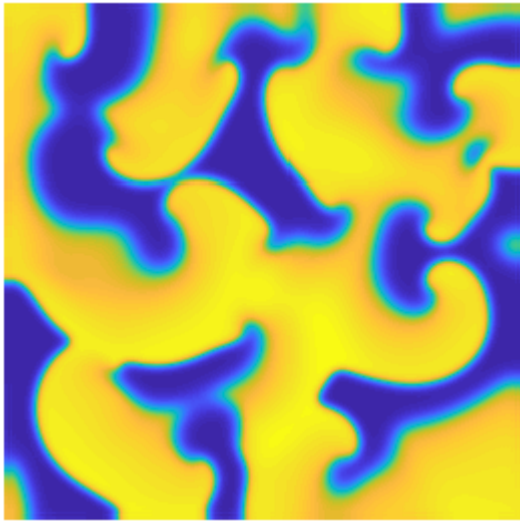
Step 4: signed distance function



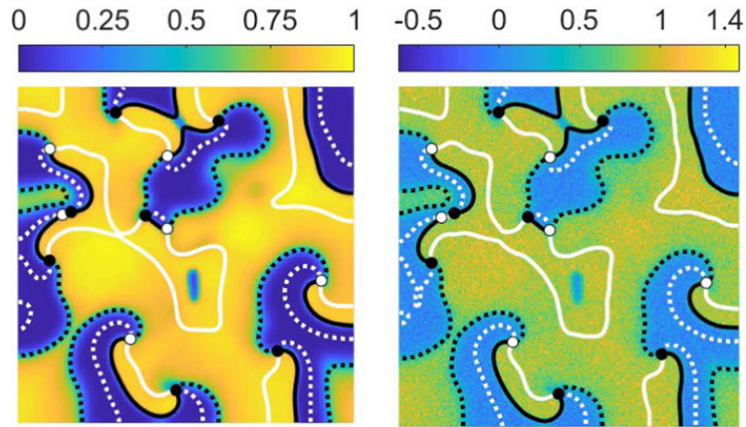
Step 5: smooth level sets



Dealing with sparsity

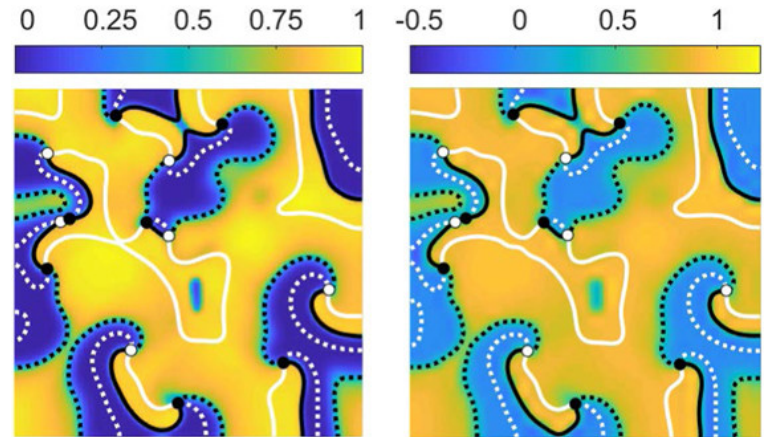


Effect of noise and sparsity



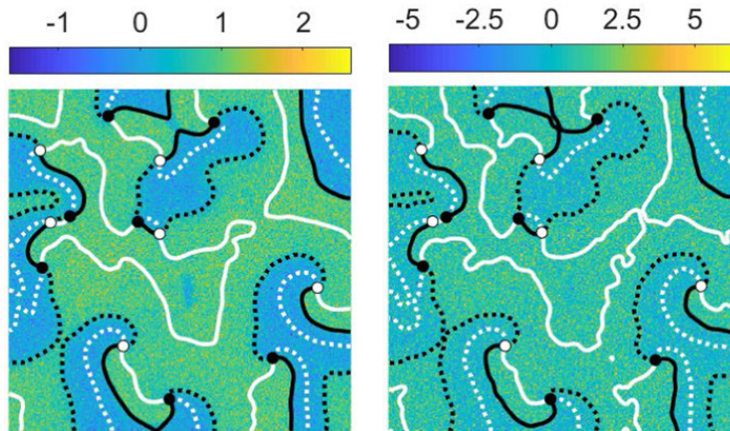
(a)

(b)



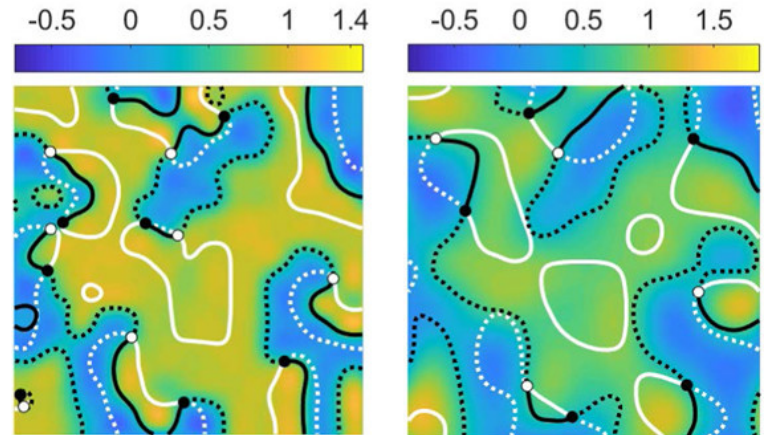
(a)

(b)



(c)

(d)



(c)

(d)

Full resolution, noise level $\eta=0, 0.1, 0.3, 1$

No noise, spatial grid 256x256, 32x32, 16x16, 8x8

Effect of noise and sparsity

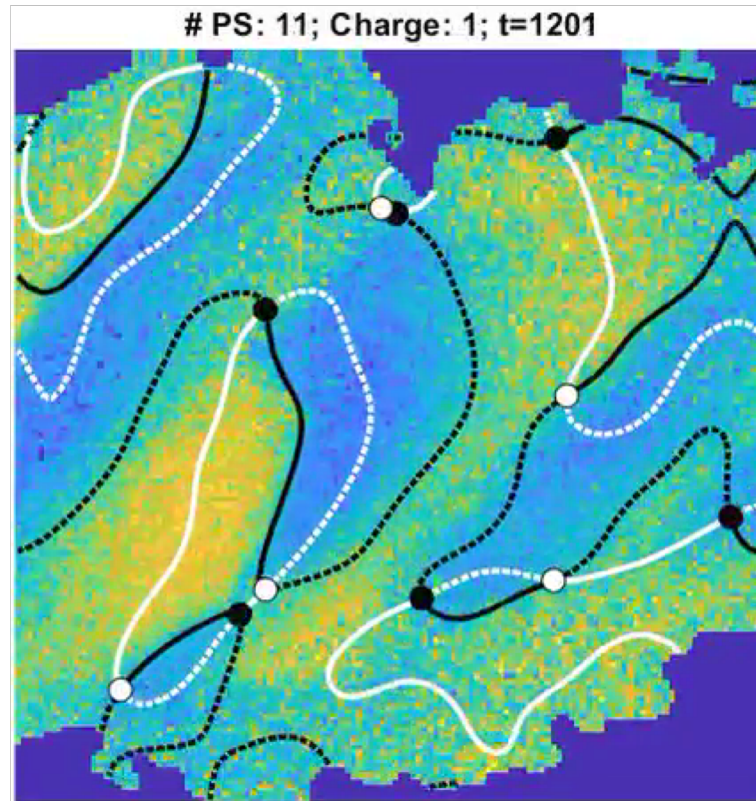
| | 256x256 | 64x64 | 32x32 | 16x16 | 8x8 |
|------------|---------|-------|-------|-------|-------|
| $\eta=0$ | 0.995 | 0.995 | 0.994 | 0.955 | 0.255 |
| $\eta=0.1$ | 0.993 | 0.994 | 0.992 | 0.957 | 0.308 |
| $\eta=0.3$ | 0.988 | 0.988 | 0.985 | 0.954 | 0.357 |
| $\eta=1$ | 0.990 | 0.974 | 0.849 | 0.695 | ... |

Accuracy of PS detection
(fraction matched)

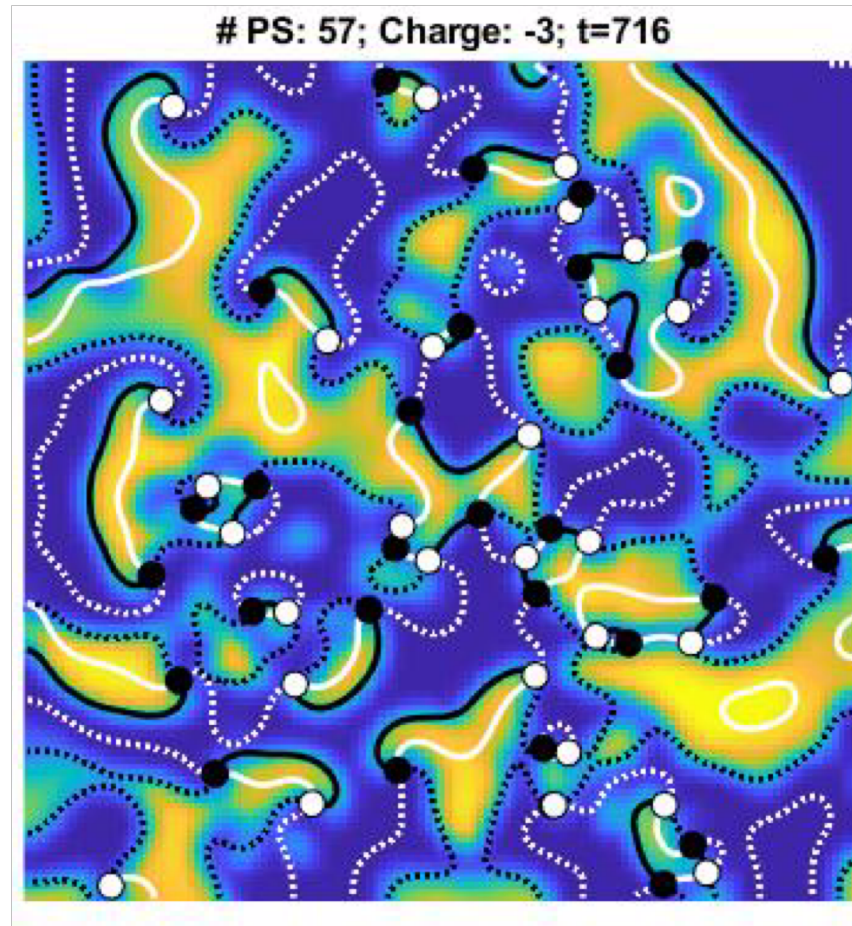
| | 256x256 | 64x64 | 32x32 | 16x16 | 8x8 |
|------------|---------|-------|-------|-------|-----|
| $\eta=0$ | 1.1 | 1.1 | 1.4 | 4.8 | 9.9 |
| $\eta=0.1$ | 1.2 | 1.3 | 1.6 | 4.6 | 9.6 |
| $\eta=0.3$ | 1.7 | 1.8 | 2.3 | 4.9 | 9.4 |
| $\eta=1$ | 2.3 | 3.1 | 4.5 | 6.9 | ... |

Precision of PS detection
(in fine grid units)

Ventricular fibrillation (pig)

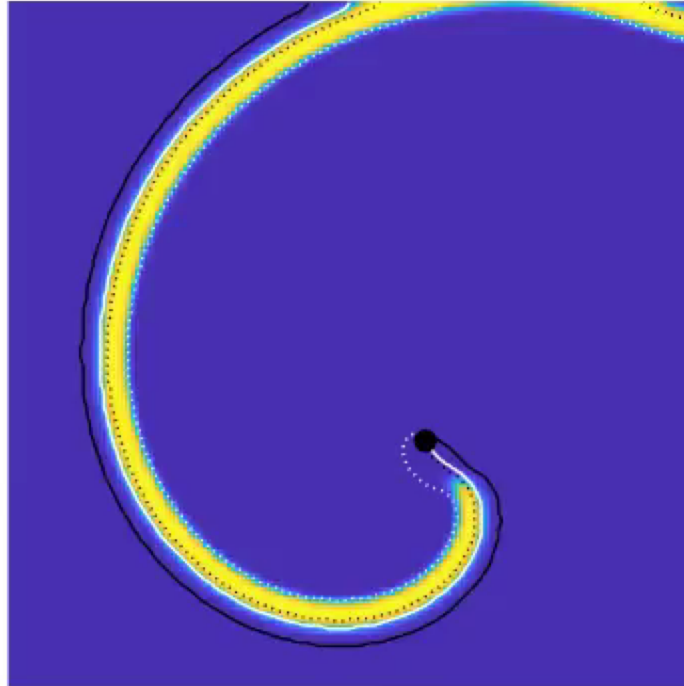


More spirals? (Fenton-Karma model)



Sparse spiral (Barkley model)

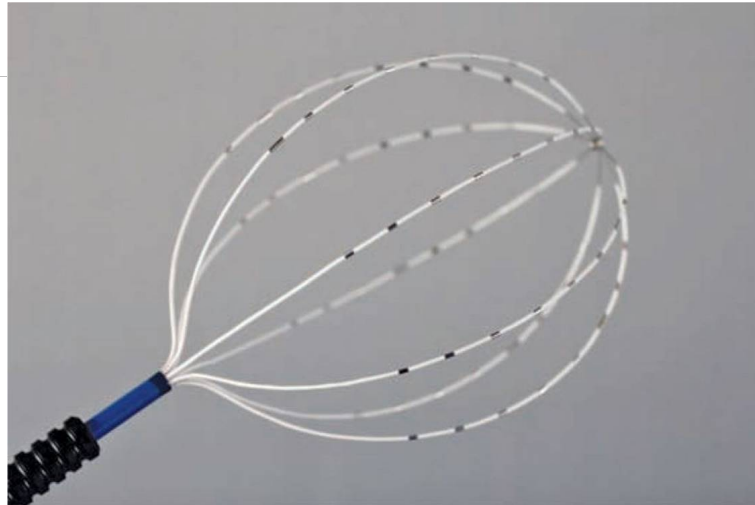
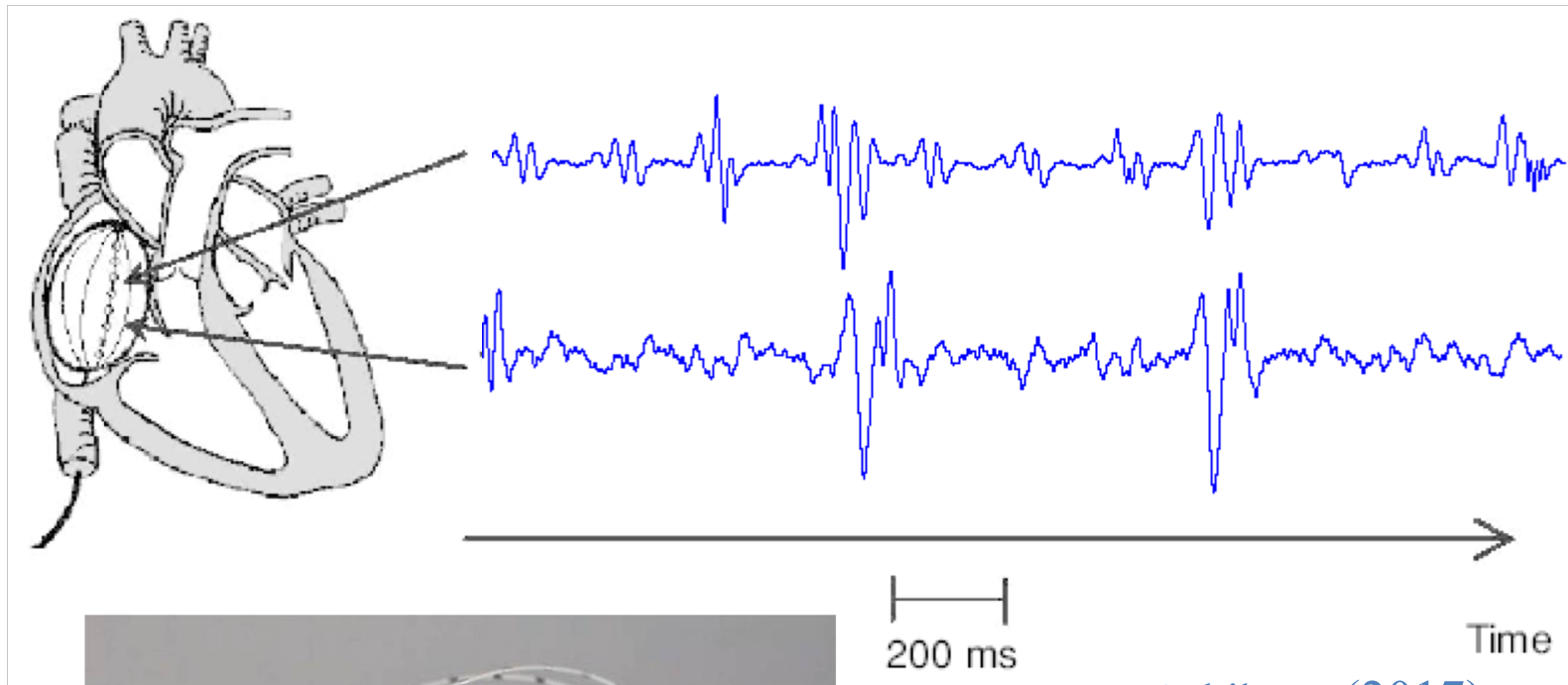
PS: 1; Charge: 1; t=1



Summary

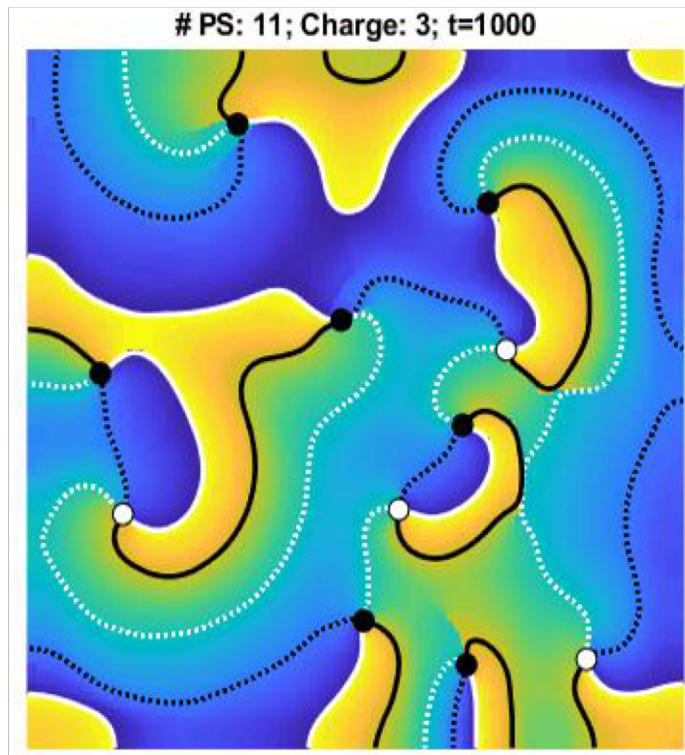
- Developed, implemented, and validated novel topological analysis of excitable systems
- This method is far more robust than existing techniques and directly applicable to numerical models and optical mapping recordings
- Can find and track many nonstationary PSs simultaneously and handle challenging edge cases
- The new approach promises to provide new insight into dynamical mechanisms underlying fibrillation

Rotor mapping for ablation therapy

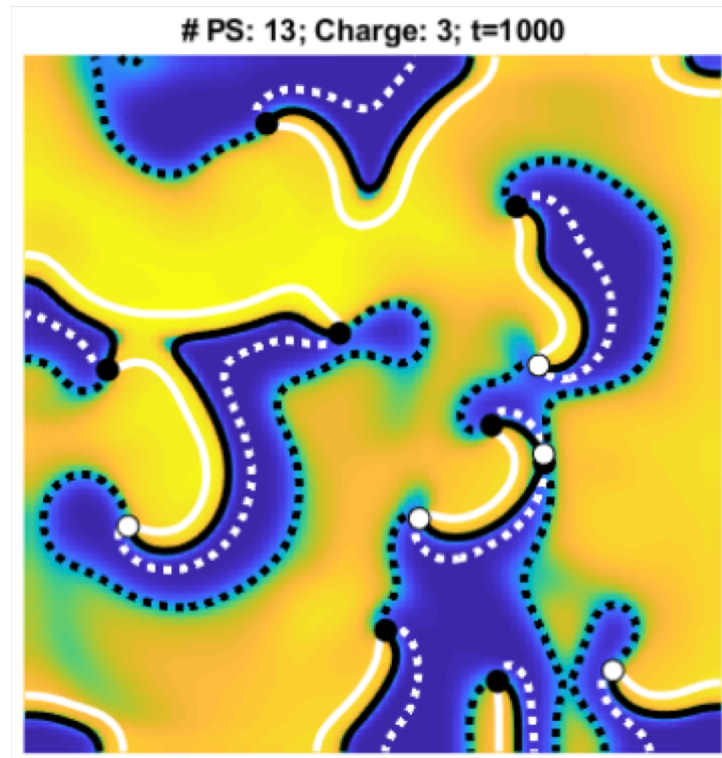


Ashikaga (2017)

Phase singularities & level sets



Level sets of phase



Level sets of voltage

Thank you!