

# Bilevel learning with applications to accelerated MRI

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## Learning parts of a variational model

In practice,  $F$  is often based on a training set of clean images and corresponding measurements  $\{u_i^*, y_i\}_{i=1}^n$ :

$$F(u_1, \dots, u_n, p) = \frac{1}{n} \sum_{i=1}^n \ell(u_i, u_i^*) + g(p).$$

Bilevel optimisation problems are hard to solve: regardless of whether the objective function is convex, the problem is usually nonconvex as the constraint set is nonconvex.

## Some previous work on bilevel learning

De los Reyes, Schönlieb, and Valkonen 2017: Learning optimal denoising parameters  $p = (\alpha, \beta)$  for higher order regularisation methods, with theoretical results in the function space setting.



(a) Clean image



(b) Noisy image



(c) Denoised image

## A different but related approach

Rather than look at the reduced problem, we could look at the following problem (Domke 2012; Ochs et al. 2016)

$$\min_p F(u^{\text{alg}}(p), p).$$

Tools for automatic differentiation such as Tensorflow allow for easy computation of derivatives of  $u^{\text{alg}}$ .

- Hammernik et al. 2017: Variational networks, inspired by the fields of experts model, for accelerated MRI reconstruction,
- Adler and Öktem 2017: learned gradient descent and learned primal-dual algorithms for inverse problems.



# Magnetic Resonance Imaging



(a) An MRI machine in operation



(b) An image of a knee acquired by MRI

We model the (fully sampled) measurements  $y$  taken by the MRI machine as

$$y = \mathcal{F}u^* + \varepsilon$$

and reconstruct the image from measurements  $\text{diag}(S)y$  by minimising a TV-regularised least squares functional:

$$\hat{u} = \underset{u \geq 0}{\text{argmin}} E_{\text{TV}}(u, y, S, \alpha) := \frac{1}{2} \|\text{diag}(S)(\mathcal{F}u - y)\|_2^2 + \alpha \|\nabla u\|_1.$$

# Total variation regularisation

Total variation regularisation (Rudin, Osher, and Fatemi 1992) gives a smoothing effect, while preserving edges.

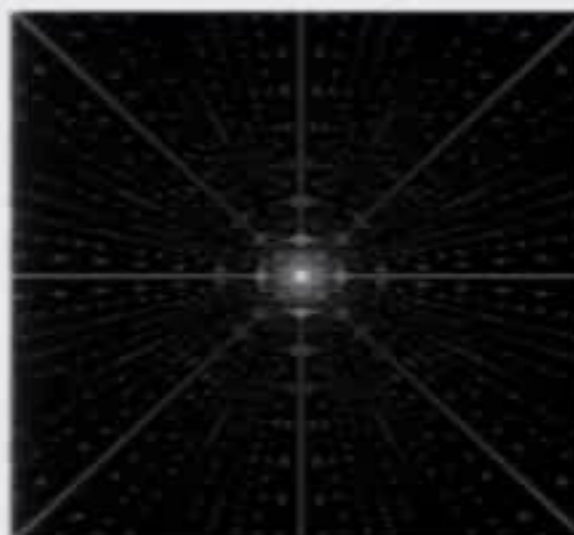


# The effect of the sampling pattern

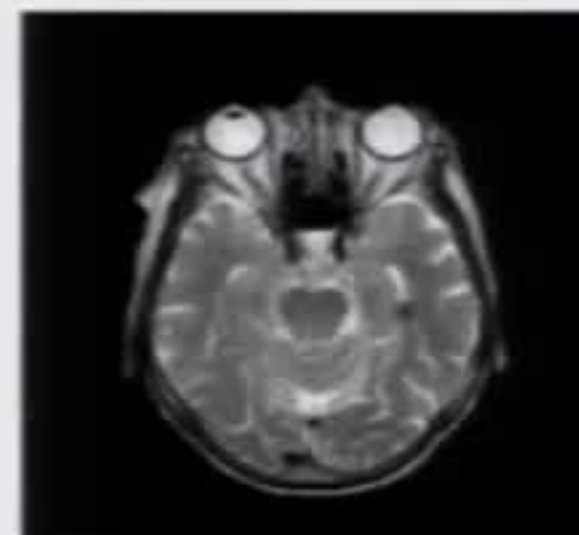
Ground truth



Radial lines, ~3%



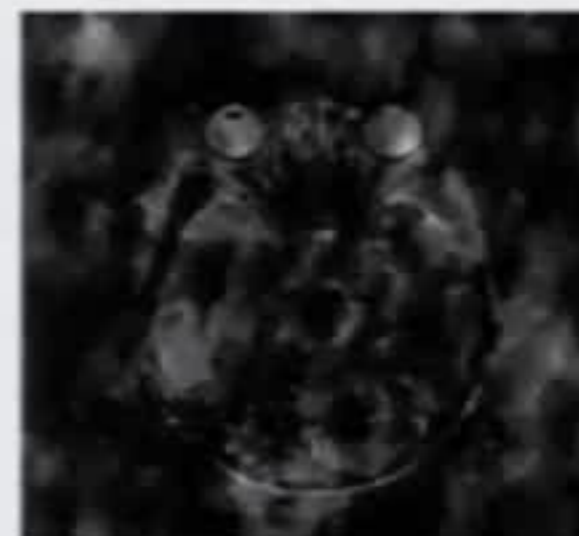
TV Reconstruction



Uniformly random, ~10%



TV Reconstruction



(Krahmer and Ward 2014; Poon 2016)

# Solving the bilevel problem

We can now put together the parts that we saw before to get an algorithm to learn a sampling pattern:

- The LBFGS-B algorithm can be applied since the problem is smooth with box constraints.
- To compute the required gradients, we solve a large linear system, so we use an iterative solver such as GMRES.
- The objective function splits as sum over the training set, so computations can easily be parallelised or randomised.



## Some preliminary results

A training set consisting of a single image of a square with resolution  $64^2$ .



(a) Clean image



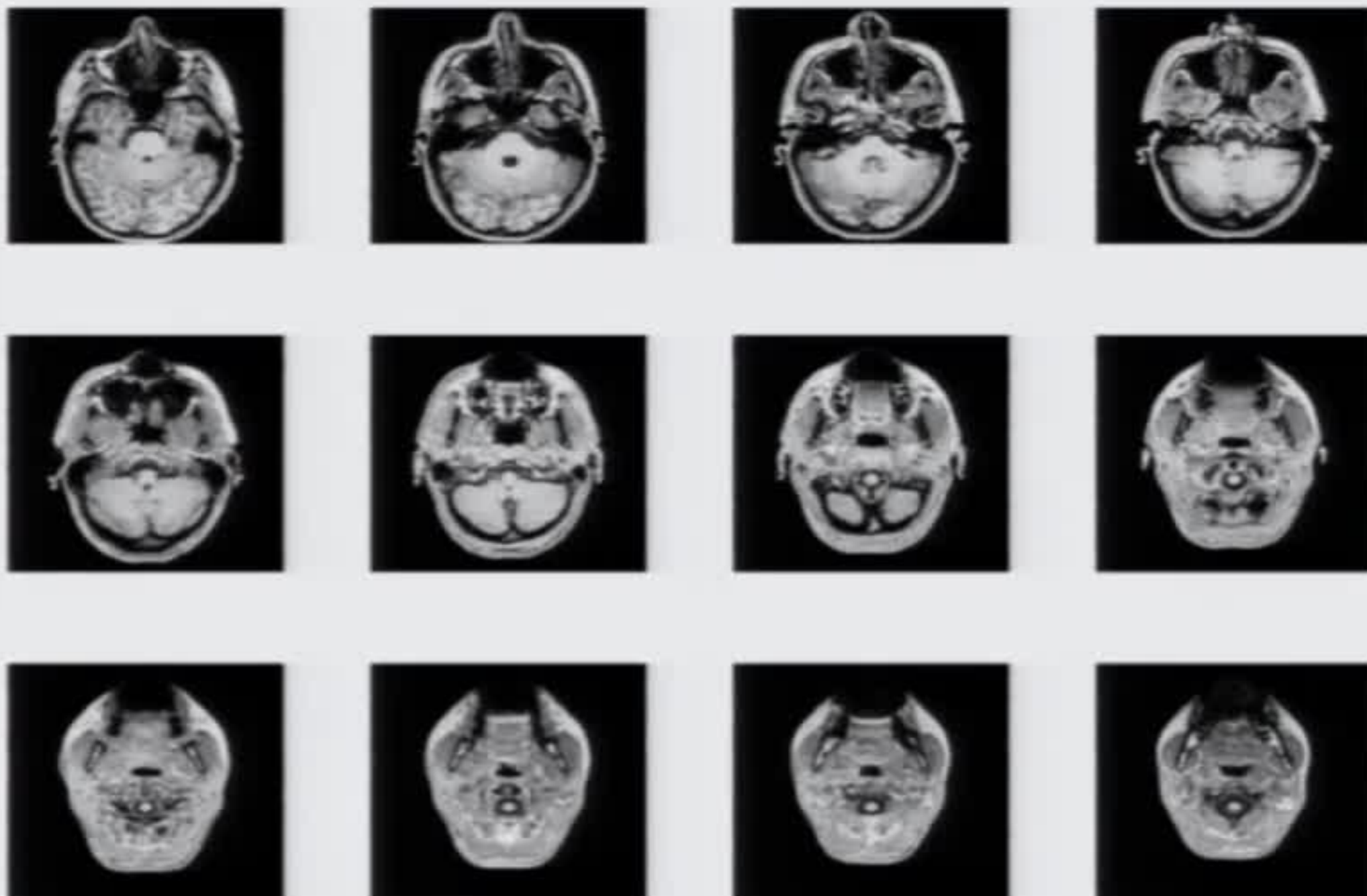
(b) Learned pattern



(c) Reconstruction

## Some preliminary results

We use a training set of size 12, consisting of brain MRI images of resolution  $192^2$  taken at Addenbrooke's Hospital in Cambridge



## Some preliminary results

Learned sampling pattern, 4%



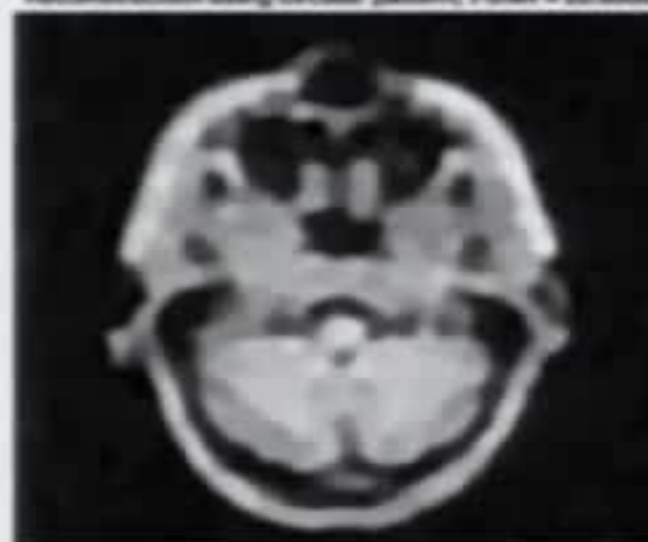
Reconstruction using learned pattern, PSNR = 21.3232



Circular sampling pattern, 4%



Reconstruction using circular pattern, PSNR = 20.5900



Better comparisons should be possible with less sparse sampling patterns.

## Summary and future work

Bilevel optimisation problems pop up naturally when learning parts of a model. We have proposed a bilevel optimisation problem to learn a sampling pattern for MRI and an approach to try to solve it. We still need to

- Compare to other methods for choosing sampling patterns,
- Study the effect of different regularisations in lower level problem,
- Study sensitivity of the learned sampling pattern to changes in the training set,
- Investigate the use of stochastic optimisation methods to scale up to large training sets,
- Investigate ways to incorporate physical constraints imposed by the MRI machine.